

GafChromic Protocol

Multi-Channel Film Dosimetry + Gamma Map Analysis

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Ashland proprietary patented technology



GafChromic Film for Dose Measurement

➔ Radiotherapy (MV photons-electrons-protons)

- EBT2, EBT3, EBT3+, EBT3P (1 cGy to >40 Gy)
- EBT-XD 4x EBT3 Dose (**New** 2015)
- MD-V3 10x EBT Dose
- HD-V2 100x EBT Dose

➔ Radiology (kV photons)

- XR-RV3 - 5 cGy to 15 Gy
- XRQA2 - 1 mGy to 20 cGy



GafChromic Protocol

➤ Advantages of GafChromic Film

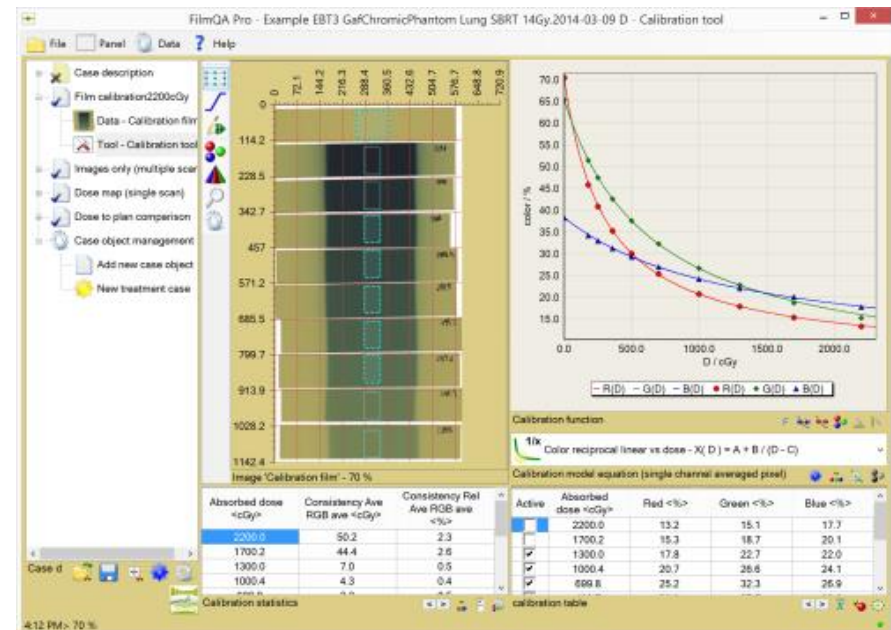
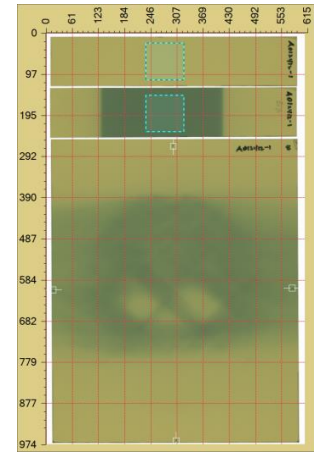
- High spatial resolution
- Wide dynamic dose range

➤ Achievements

- Accuracy of 0.5% dose error
- Efficient work flow
- Active error recognition

➤ Protocol Elements

- GafChromic Film
- FilmQA Pro
- Multi-channel film dosimetry with rescaling
- Quick Phantom



GafChromic Protocol

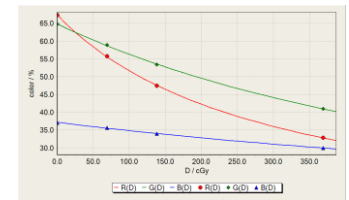
➤ Exposure and Scanning Procedure

- Film handling using GafChromic Quick Phantom
- Avoidance of measurement disturbances



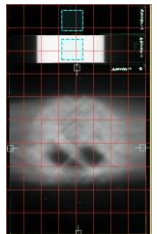
➤ Primary Calibration

- Efficient way to generate calibration
- Adaptive calibration for specific measurements



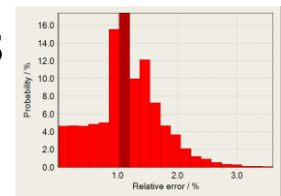
➤ Measurement Evaluation

- Multi-channel dosimetry with calibration optimization
- Dose error estimation and active measurement design



➤ Dose Comparison

- Parameterized comparison with sensitivity analysis
- Feedback for measurement improvements

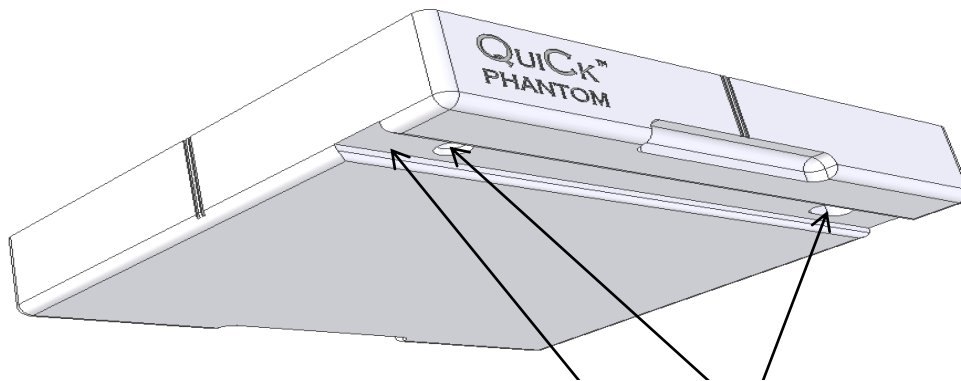


GafChromic Protocol

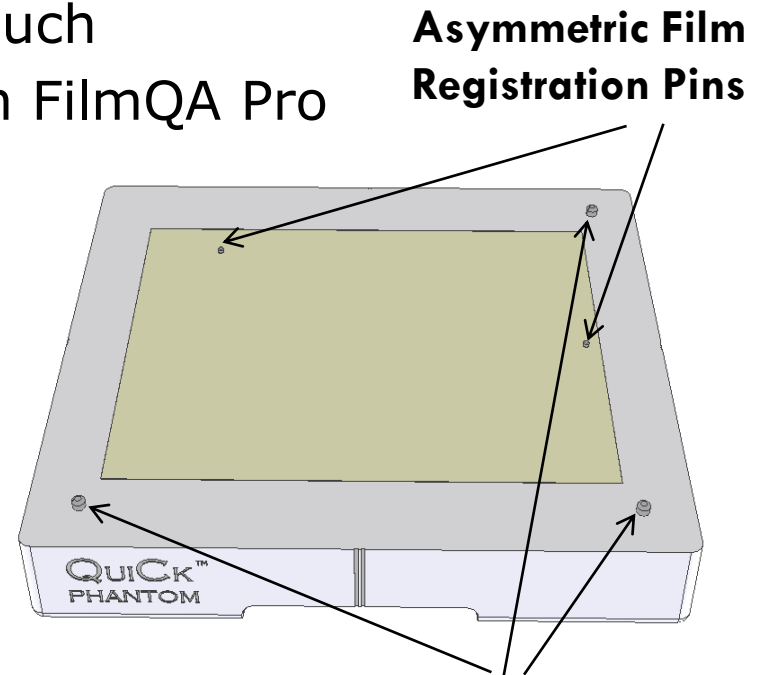
Exposure Procedure

GafChromic Quick Phantom

- Two Plastic Water[®] slabs
- Forced positioning on couch
- Automatic registration in FilmQA Pro
- Use with **EBT3P**



Groove and two holes to fit standard two Pin patient positioning index bar

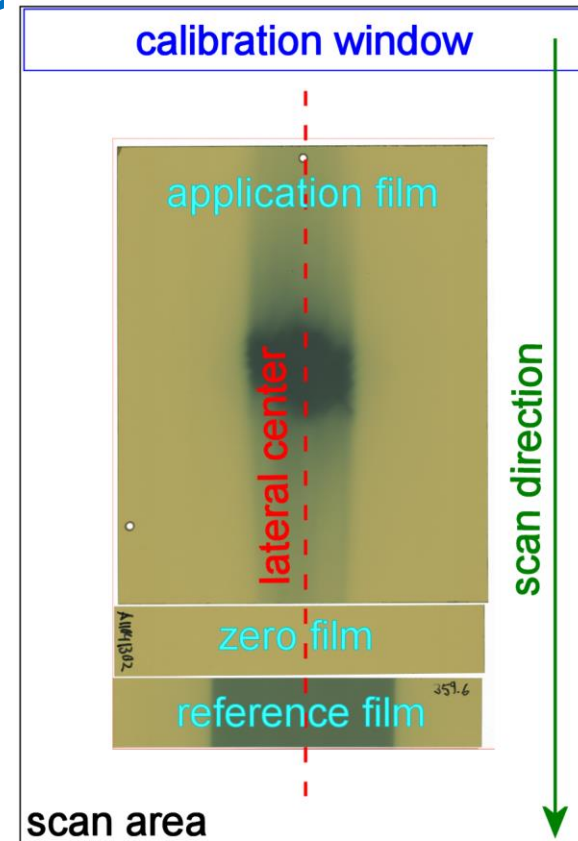


Top Plate Locking Dowel Pins

GafChromic Protocol

Scanning Procedure

- ➔ Film Positioning on Scanner
 - Highest dose at lateral center
 - Most of exposed areas at lateral center
- ➔ Flatten Film on Scanner
 - Use Glass Plate on top of all films
 - Cover scanner calibration window
 - No masks, No film overlap
 - Silica particles at EBT3 surface suppress Newton rings
- ➔ No Color Correction, 72 dpi, 48 bpp
- ➔ Same orientation of all Films



GafChromic Protocol

Primary Calibration

➤ Single calibration scan

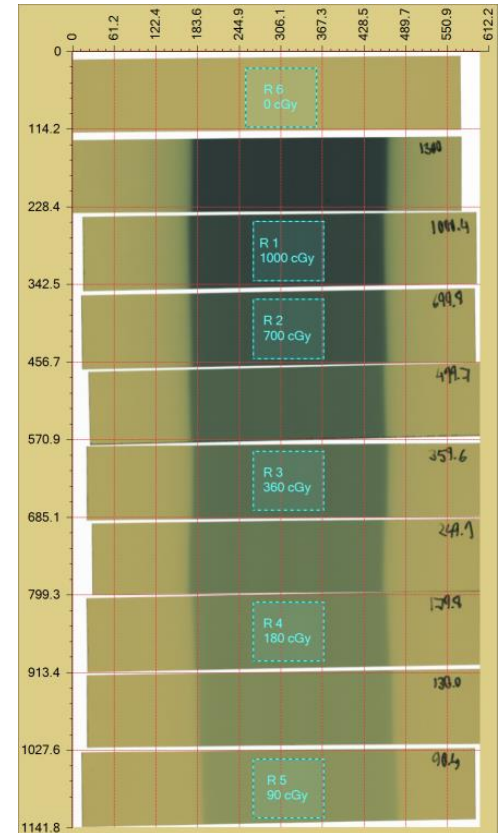
- 9 exposed strips with *geometric* dose sequence + unexposed strip
- Single scan avoids scan to scan variations

➤ Optimize for specific measurement

- Use only dose values relevant for measurement $<(\text{max dose} + 10\%)$
- Select 3-5 exposures + unexposed film

➤ Calibration criterion

- Minimize dose error (best consistency)
- Correlate only 'Shape' of functions



Active	Absorbed dose <cGy>	Red <%>	Green <%>	Blue <%>
<input type="checkbox"/>	2200.0	13.2	15.1	17.7
<input type="checkbox"/>	1700.2	15.3	18.7	20.1
<input checked="" type="checkbox"/>	1300.0	17.8	22.7	22.0
<input checked="" type="checkbox"/>	1000.4	20.7	26.6	24.1
<input checked="" type="checkbox"/>	699.8	25.2	32.3	26.9
<input checked="" type="checkbox"/>	499.7	30.0	37.5	29.2
<input checked="" type="checkbox"/>	359.6	35.1	42.6	31.2
<input type="checkbox"/>	249.9	40.7	47.5	32.9
<input type="checkbox"/>	179.8	45.8	51.4	34.2
<input checked="" type="checkbox"/>	0.0	70.4	65.3	38.3

GafChromic Protocol

Measurement Evaluation

➤ Application Film

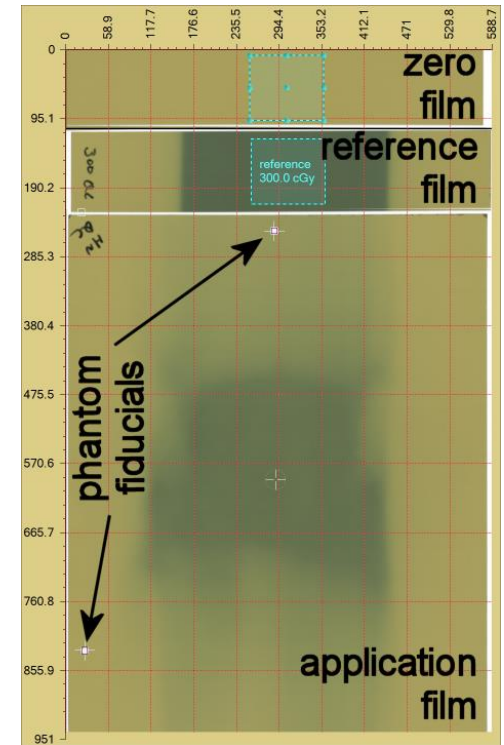
- Optimize calibration's dose range

➤ Reference Film

- Reference dose at 'dose range of interest'
- Recommended reference dose $\sim(\text{max dose} - 15\%)$
- Multiple references possible to adjust best accuracy range

➤ Zero Film

- Do Not use dedicated strip



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Measurement Evaluation

➤ Verify Reference Film

- Reference patch has lowest dose error
- Rescaling correction $\ll 5\%$ otherwise reference inconsistent

➤ Verify Dose Accuracy

- Screen 'dose area of interest' in consistency map (dose error)
- Watch for artefact pattern e.g. lifted film corners

Dose map (single scan)

Dose map (single scan)

Dose map: Dose map using triple channel uniformity

Recalibration: Dose linear scaling

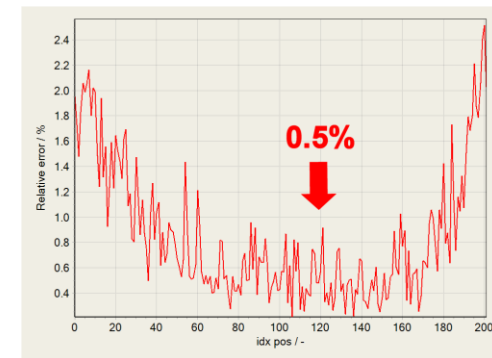
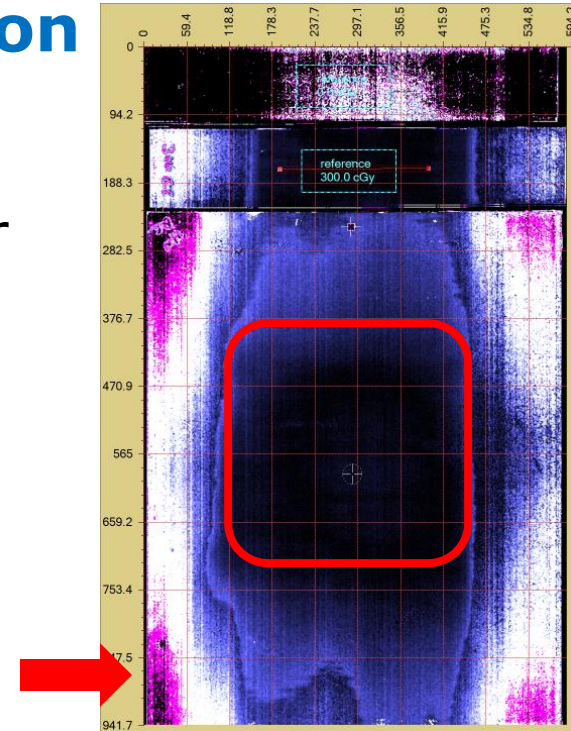
References 1300.0 / 699.8 / 1000.4 / 0.0 cGy

Recalibration parameter:

Red = A = 0.014 , B = 1.016

Green = A = 0.030 , B = 1.014

Blue = A = 0.118 , B = 1.022



GafChromic Protocol

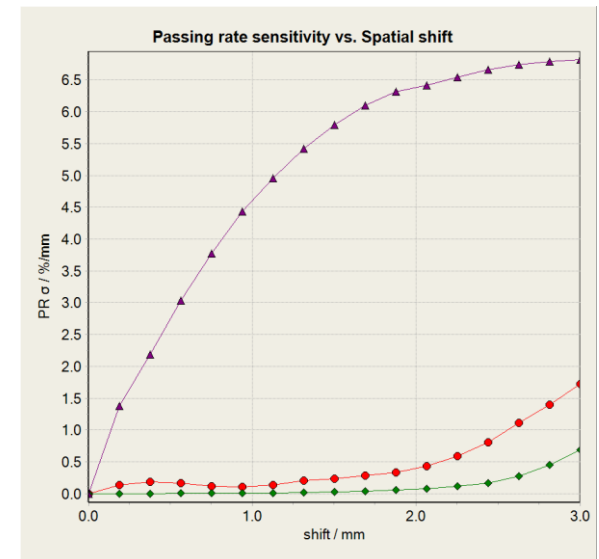
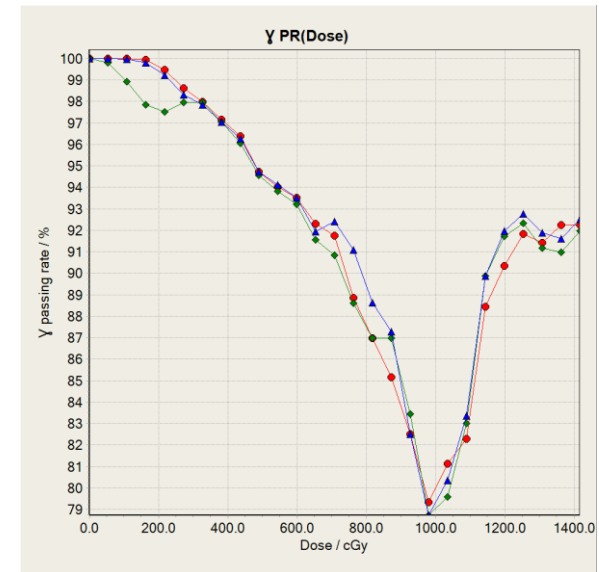
Dose Comparison

➔ Advanced Comparison

- Chart Passing Rate vs parameters
- RGB Passing Rates must be consistent
- Chart Passing Rate vs Dose recognize calibration bias
- Optimize calibration

➔ Comparison Sensitivity

- Assure comparison is sensitive to targeted QA
 - e.g. spatial shift



Multi-Channel Calibration

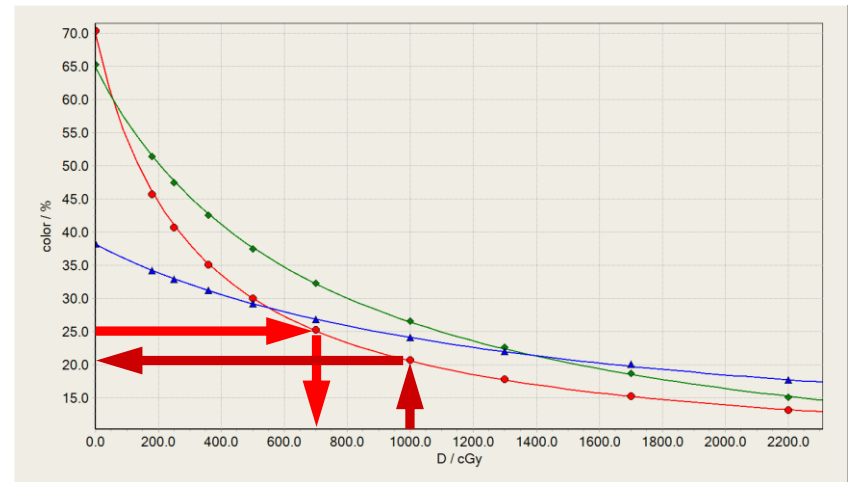
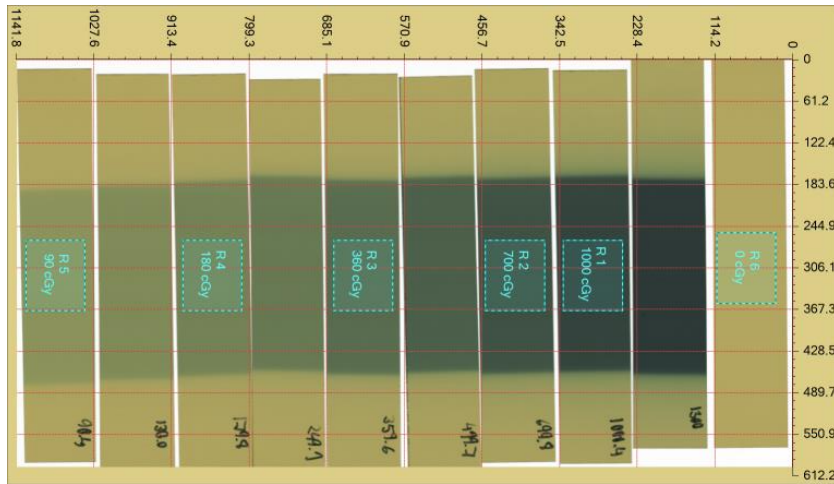
➤ Correlates average response

- System: **Radiation machine – Film - Scanner**
- Fixed protocol conditions: *dose range, ambient, scanner state*
- Mode of operation: *film orientation, scan glass plate*

➤ Dose vs Color Channels X=RGB (optical density)

$$D = D_X(X_{ave}) \leftrightarrow X_{ave} = X(D)$$

$$D = D_X(d_{X,ave}) \leftrightarrow d_{X,ave} = d_{X,D}(D) \quad (d_X = -\ln_{10}(X))$$



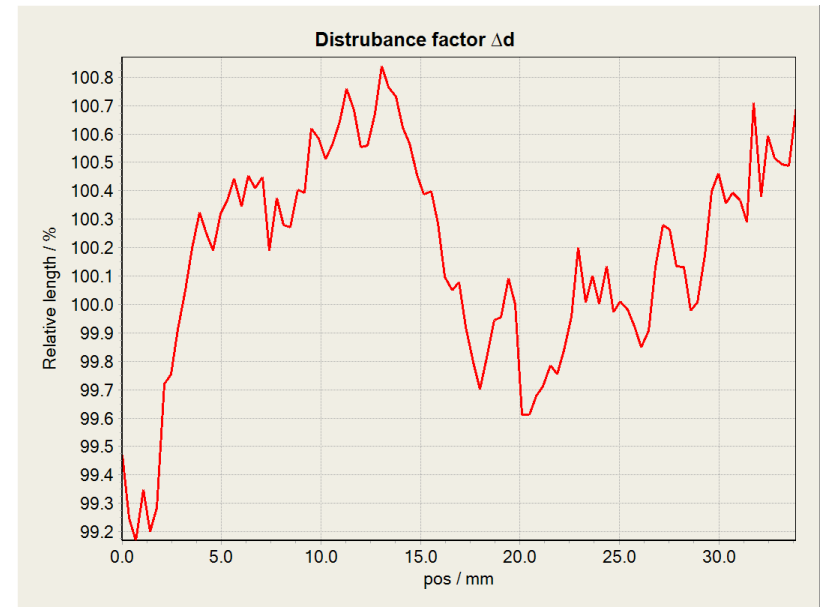
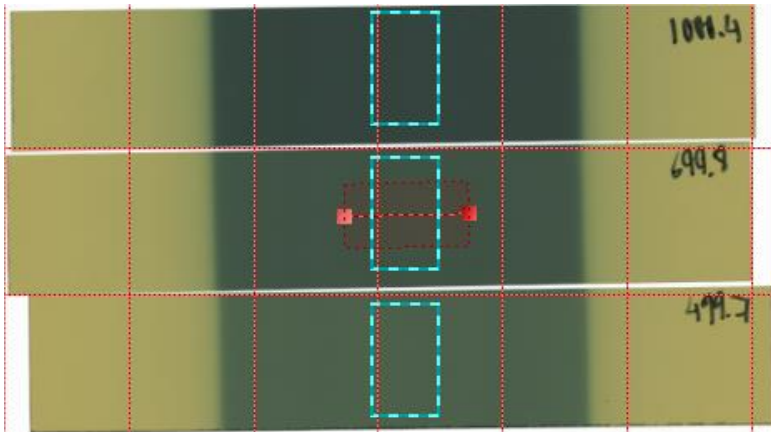
Multi-Channel Calibration

→ Disturbance Factor

$$\Delta d = \frac{d_{X,scan}(D)}{d_{X,ave}(D)} = \frac{\text{specific response}}{\text{average response}} @ \textit{same dose}$$

→ Example: Calibration Strip

- Calibration region all pixel have same (known) Dose
- Major contribution to Δd film non-uniformity
- Δd neutral with respect to X



Multi-Channel Dosimetry

→ Dose Calculation

$$d_{X,scan}(D_X) = d_{X,ave}(D_X)\Delta d$$

- Disturbance factor connects D_X dose calculations, $X=RGB$

→ Consistency κ

$$\kappa(\Delta d)^2 = \sum_{X \neq Y} (D_X - D_Y)^2$$

- Consistency is dose offset averaged at single location

→ Only 1 Dose at each location

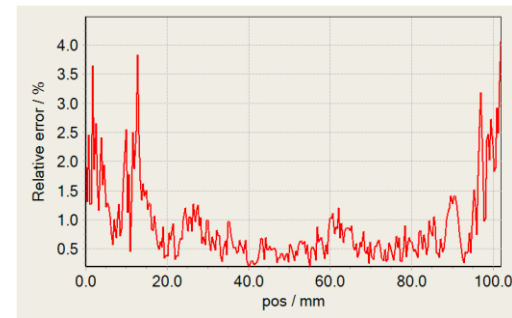
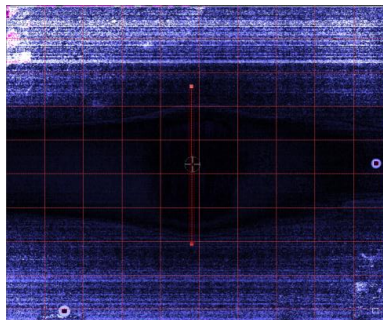
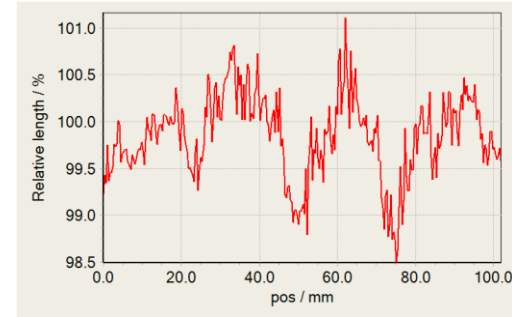
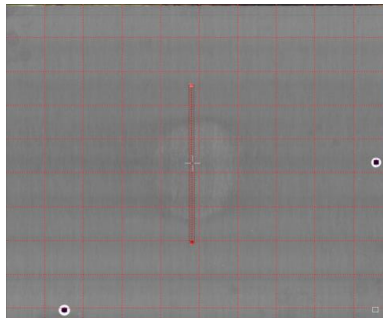
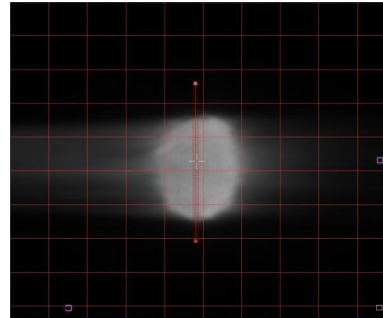
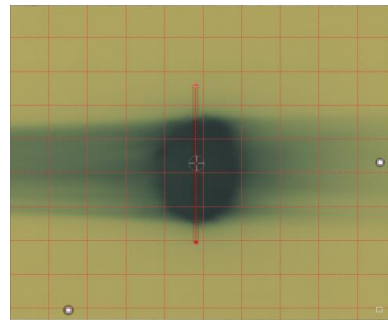
- Dose calculation must deliver same value, i.e.

$$\kappa(\Delta d) \rightarrow \min_{\Delta d}$$

- Find Disturbance with best consistency, perfect $\kappa \equiv 0$
- At all pixels: 4 equations, 4 variables D_X and Δd

Multi-Channel Dosimetry

➔ Signal split into *dose dependent* and *dose independent* part



Calculate Maps

- Dose - D_x
- Disturbance - Δd
- Consistency - κ

Multi-Channel Dosimetry Consistency

➤ Film with Perfect Consistency

- Film's average dose response for X=RGB identical with Calibration

➤ Imperfect Consistency

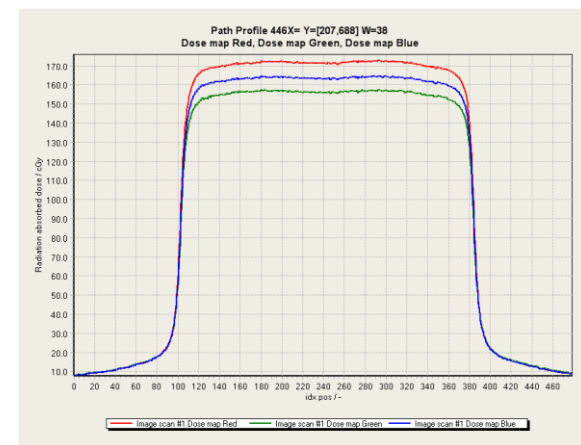
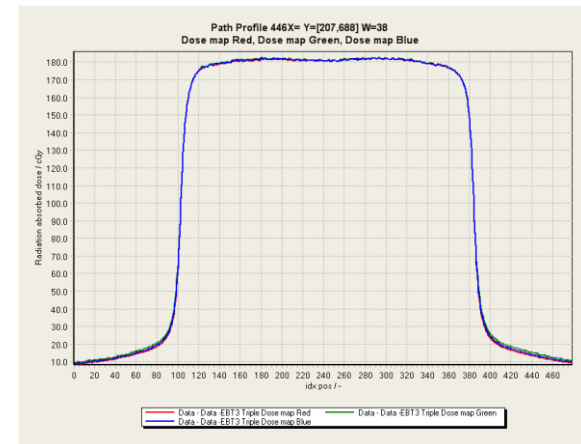
- Film's average dose response for X=RGB deviates from Calibration

➤ Assume Film has Same Response

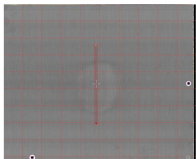
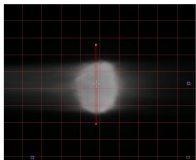
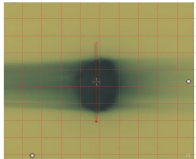
- Imperfect Consistency is measure for Dose Error
- Offset between D_x estimates Dose Error

➤ Example

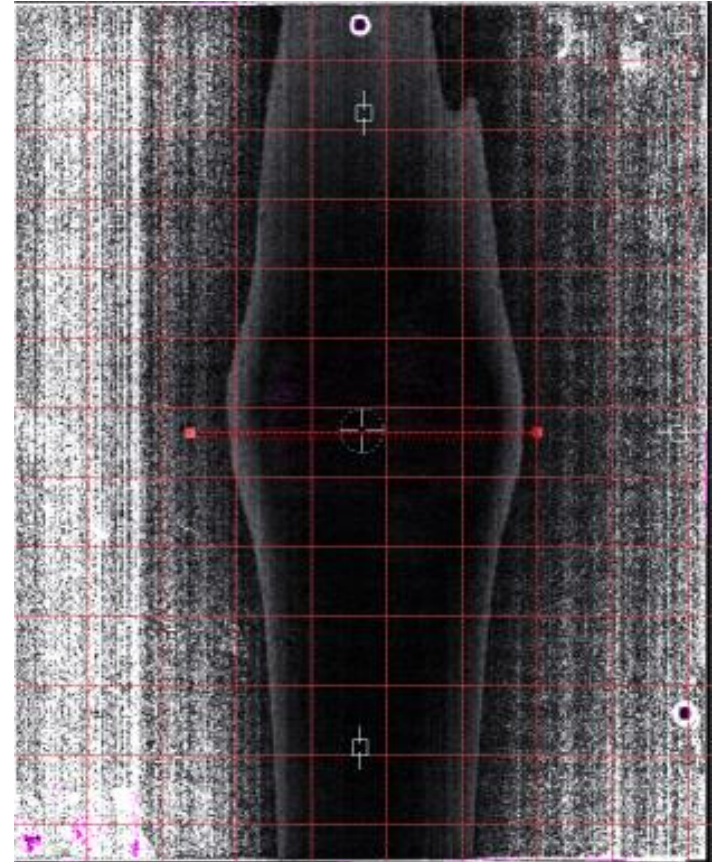
- Profiles original calibration patch and 90° rotated scan



Multi-Channel Dosimetry Consistency Map



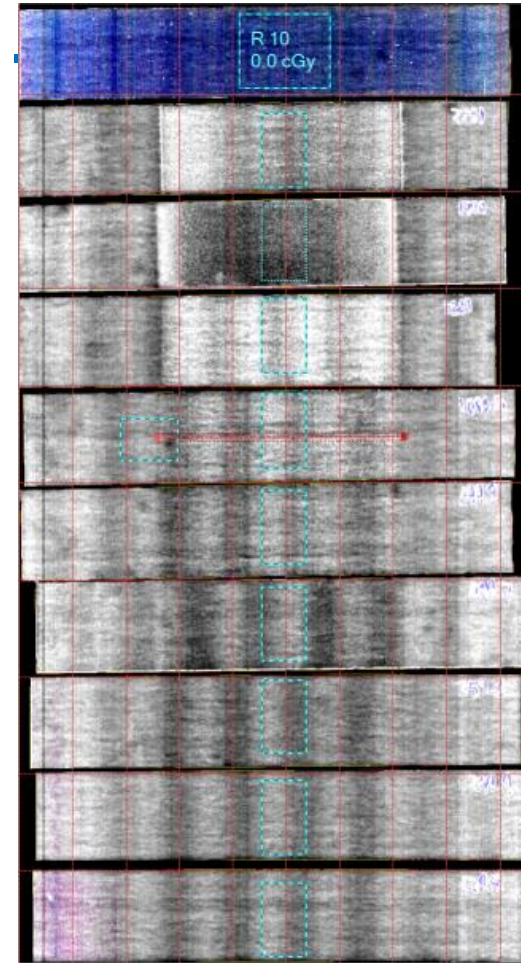
- Film scan
measurement raw data
- Dose map - D_x
measurement result
- Disturbance - Δd
removed error
- Consistency - κ
remaining error
 κ absolute error
 κ/D relative error



Example: Different sensors at different lateral position + lateral scanner effect cause (slightly) different average response.

Multi-Channel Dosimetry Disturbance Map

- Disturbance Δd - **removed error**
- Presents **relative film thickness** when Δd dominated by film non-uniformity
→ Uniformity Map
Film uniformity: spec $\pm 1\%$, typical $\pm 0.5\%$
- $|\Delta d - 1| \gg 1\%$
indication of other dominant disturbances
- Image pattern hints potential error sources
- Dose dependent disturbances mitigated
e.g. lateral effect, curled film, calibration bias



Example: Calibration scan various dose levels
(contrast advanced)

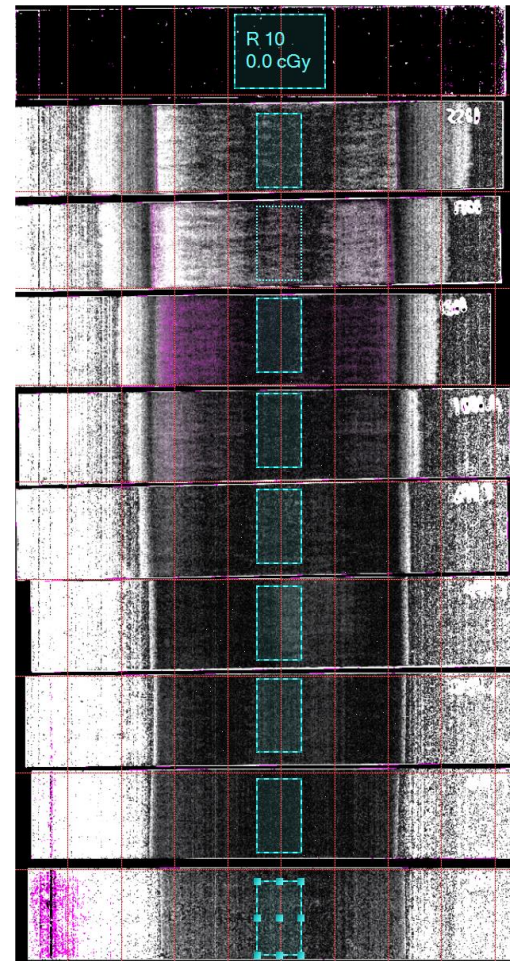
Multi-Channel Calibration

→ Optimize Calibration

- Lower consistency = better calibration
- Offset in calibration points is **not** a quality criterion
- Calibration strips must be consistent with calibration

→ Calibration goal

- Correlate calibration parameter for **Perfect Consistency** $\kappa \equiv 0$
- Calibration functions $\{ R(D), G(D), B(D) \}$ must match film dose spectrum



Optimize Consistency κ
shown relative consistency

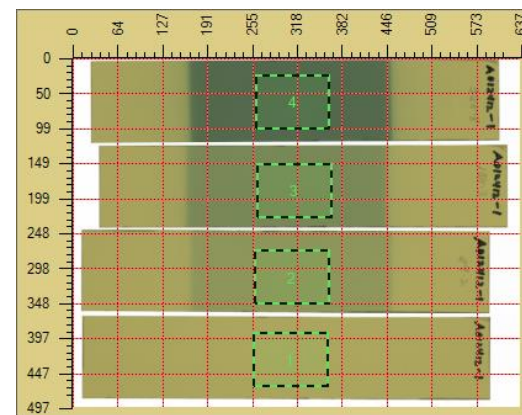
Multi-Channel Calibration

Single channel calibration average system response

- $x = x(D)$
x = RGB
each channel fitted separately

Multi-channel calibration

- $X(D) = A + B x(a + bD)$
X = RGB
rescales calibration x
a, b dose scaling, A, B color scaling
- Correlation $D_R(R_{ref}) = D_G(G_{ref}) = D_B(B_{ref})$
optimize consistency at reference points
- Compensates calibration patch distortions
if multi channel dose is used to rescale dose



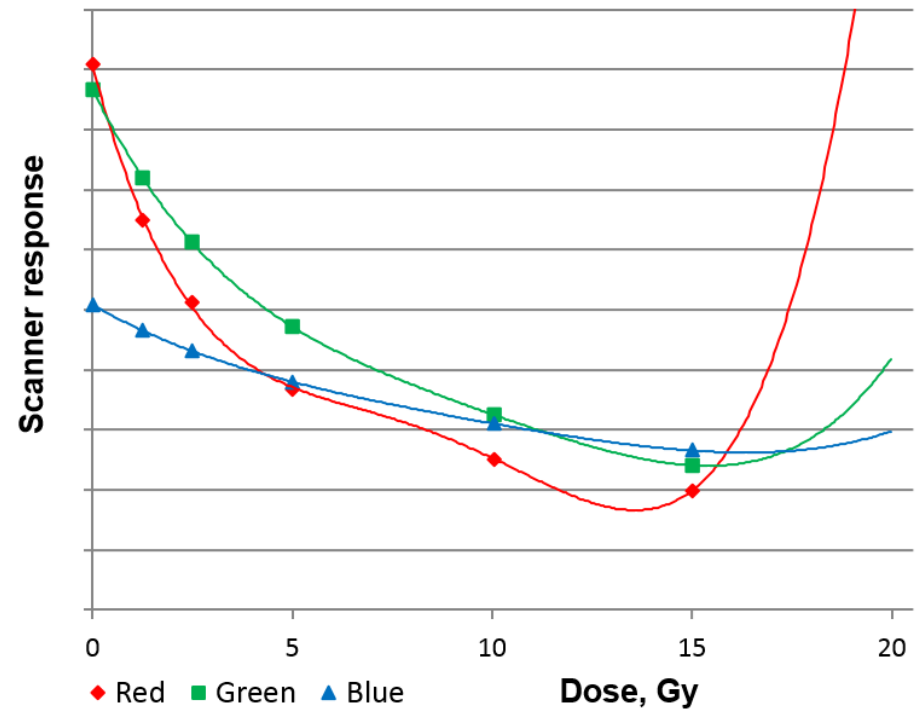
Polynomial Calibration

➤ Polynomial fit

- $x(D) = \sum A_i D^i$
- Least square solution
 $\sum (x_i - x(D_i))^2 \rightarrow \min(A_i)$
many parameters, oscillations

➤ !Do Not Use!

- Many parameters
(many calibration points)
- Non-Monotonic function
(physical incorrect!)
- Non-Invertible function
(optimization consistency at reference points costly)
- Uncontrolled behavior between calibration point
(additional calibration points to correct)



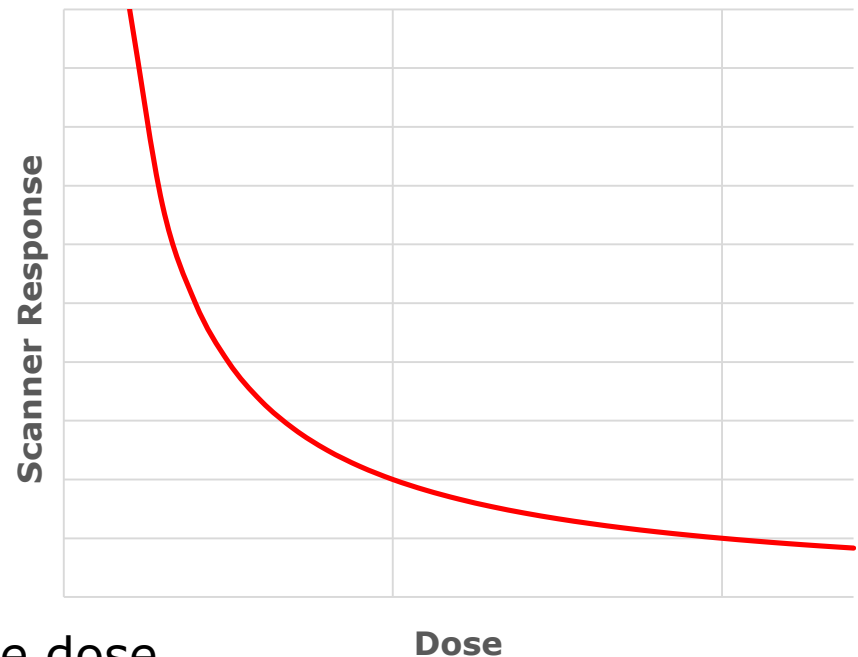
Rational Calibration

➤ Primary Calibration fits only function **Shape**

- **Example:** Reciprocal function
 $x = 1 / D$
no parameters, 'pure' shape

➤ Recalibration

- $X(D) = A + B / (C + D)$
rescales calibration x to absolute dose
- **Rational function** with 3 parameters
(only 3 dose points stipulate calibration)
- Monotonic function (always physical correct)
- Invertible function (dose vs. color) $D_x = -C + B / (-A + X)$



Multi-Channel Calibration

➤ Model functions

- Use Rational functions

Reciprocal $X(D) = A + B/(C+D)$

Linear $X(D) = (A+BD)/(C+D)$

Quadratic $X(D) = (A+BD+CD^2)/(E+D)$

➤ Optimize Consistency

- Enforce

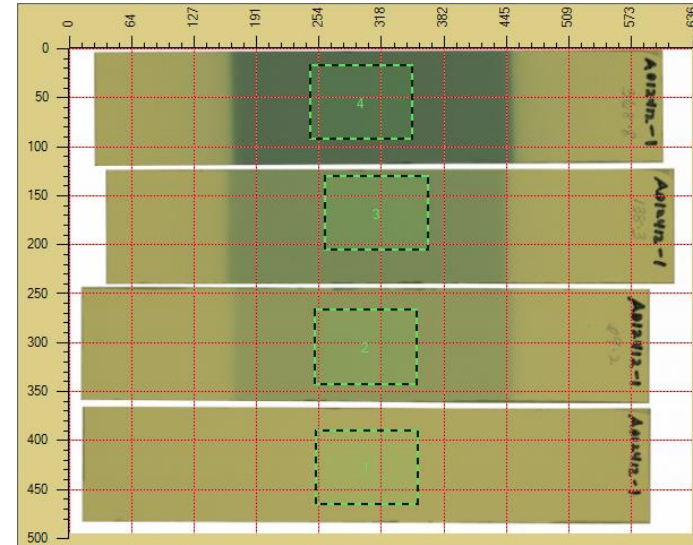
$$D_R(R_{\text{calib}}) = D_G(G_{\text{calib}}) = D_B(B_{\text{calib}}) = D_{\text{calib}}$$

for all calibration pixels X_{calib} (>10000 equations)

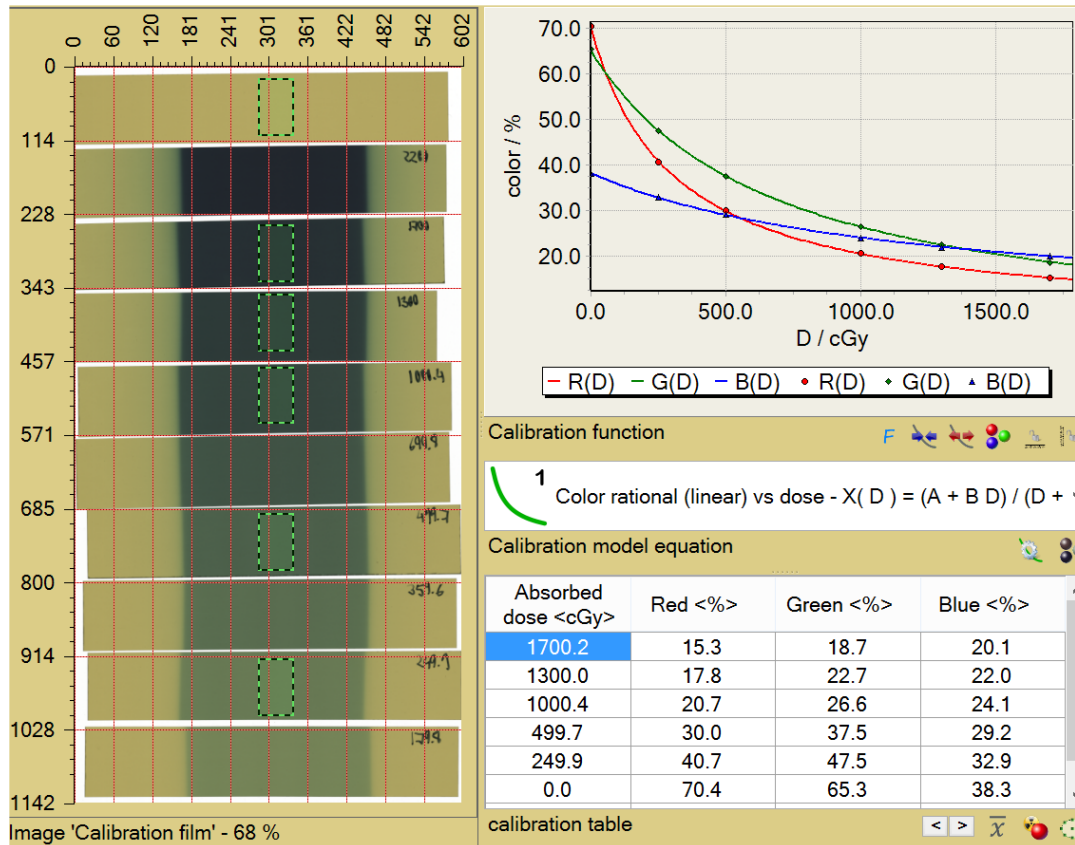
- Optimize calibration regions
- Select best model function

- **Do Not** $D_R(R_{\text{ave}}) = D_G(G_{\text{ave}}) = D_B(B_{\text{ave}}) = D_{\text{calib}}$

for all calibration dose points (<10 equations)



Multi-Channel Calibration



- **Single Calibration Scan with 10 calibration strips**
 - Use Geometric Sequence or Equal Color Steps
- **Select only patches relevant for measurement**
 - Optimize calibration to minimize dose error

Multi-Channel Calibration

➔ Two point recalibration

- 1 unexposed + 1 exposed film
Minimum cost possible
- Dose scaling ($A=0, B=1$)
 $X(D) = x(a + bD)$, $X = \text{RGB}$
- Color scaling ($a=0, b=1$)
 $X(D) = A + Bx(D)$, $X = \text{RGB}$

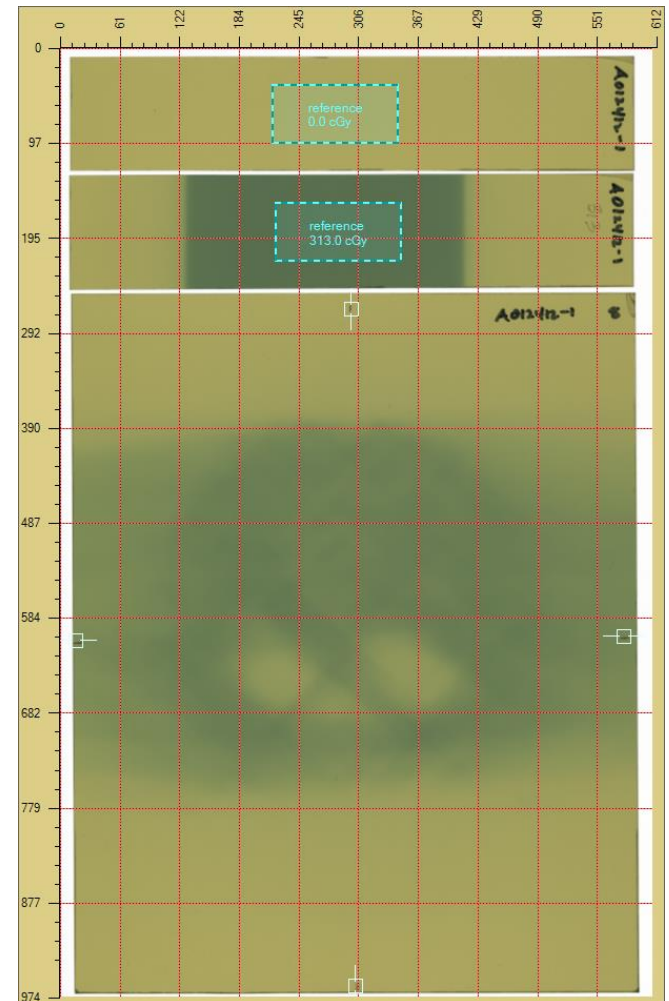
➔ Assumption

- Calibration functions keep shape
 $\text{Shape}(x) = \text{Shape}(X)$, $x, X = \text{RGB}$

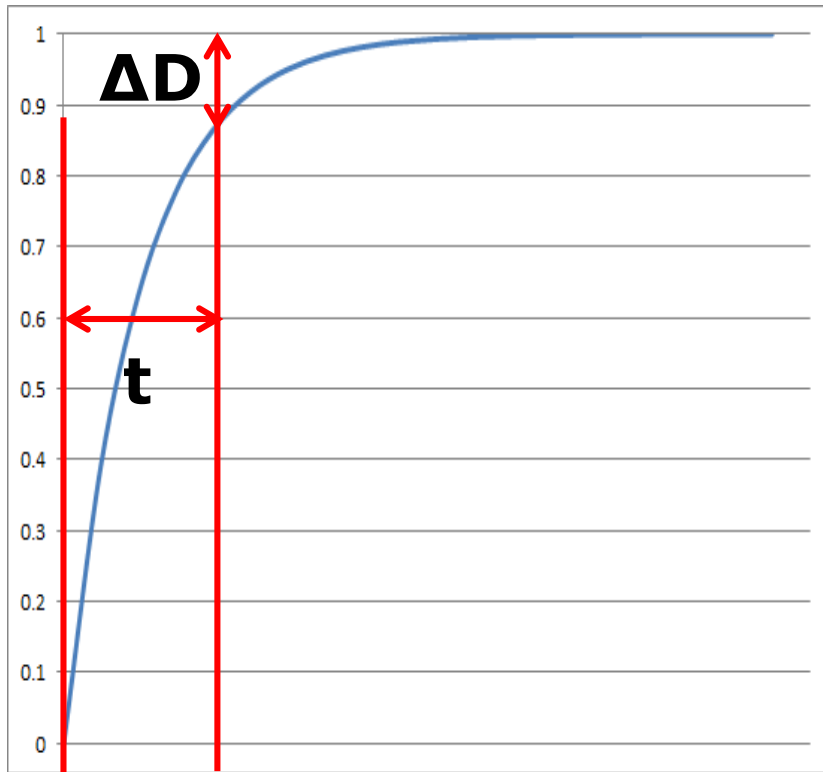
➔ Single scan Evaluation

compensates for

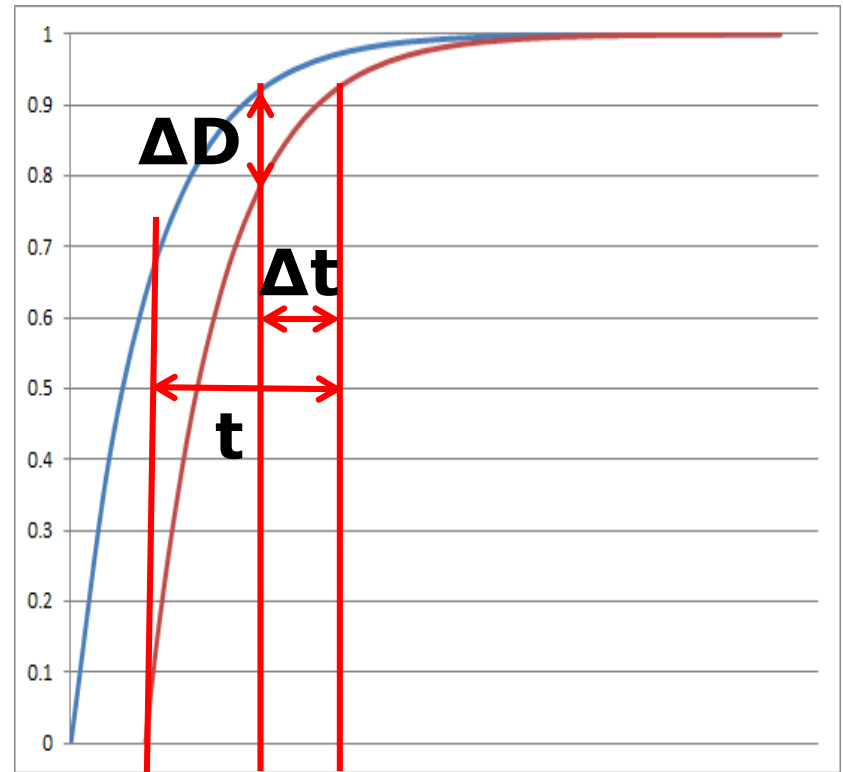
- Ambient conditions: temperature, humidity
- Inter-scan scanner variations,
- Post exposure time, film aging



Rescaling - Post Exposure Age



Absolute aging
wait $t = 24$ h
 $\Delta D(t) < 0.5\%$



Relative aging
wait $t = 4 \Delta t$
 $\Delta D(t) < 0.5\%$

Multi-Channel Calibration

→ Triple point recalibration

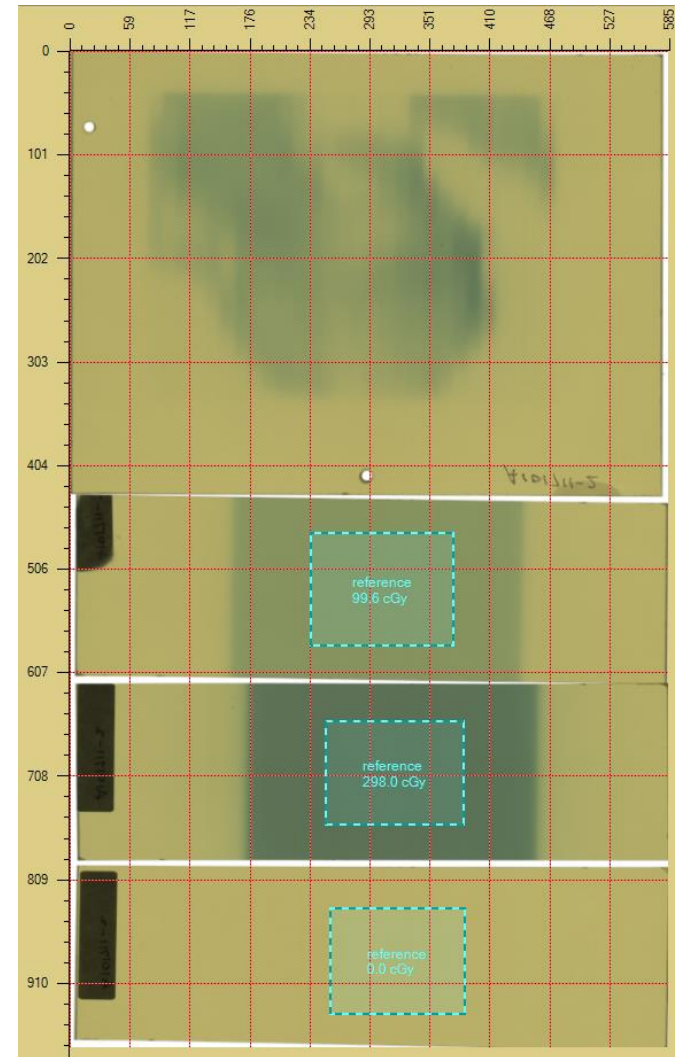
- 1 unexposed + 2 exposed film
Higher cost
- $X(D) = A + B \times (C \times D)$ (3 point rescaling)
- $X(D) = A + B \times (D^C)$
X = RGB

→ Requires 2 exposures

- Enforces perfect consistency at references
- Recalibration includes rescaling and shape correction

→ Single scan Evaluation compensates for

- All two point recalibration benefits
- Shape changing properties
i.e. any primary calibration can be used



Multi Channel Calibration

➔ Single point recalibration

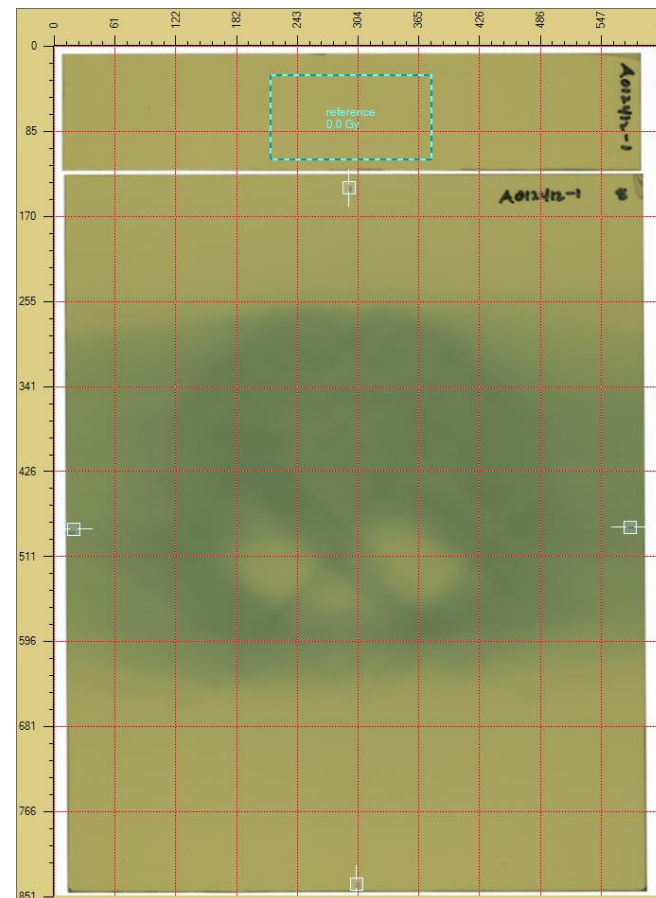
- 1 unexposed
it's **free** and always possible
- Dose shift ($A=0, B=1, b=1$)
 $X(D) = x(a + D), X = \text{RGB}$
- Color shift ($a=0, b=1, B=1$)
 $X(D) = A + x(D), X = \text{RGB}$

➔ Assumption

- Calibration functions keep shape
 $\text{Shape}(x) = \text{Shape}(X), x, X = \text{RGB}$
disturbance caused by offset only

➔ Single scan Evaluation

- compensates for
- Offset generating disturbances

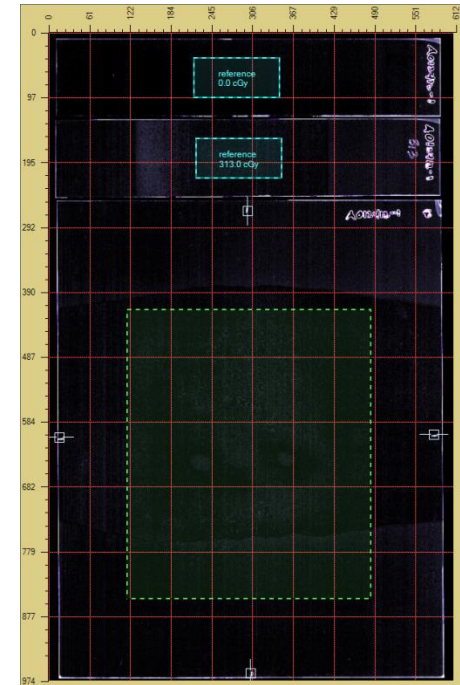
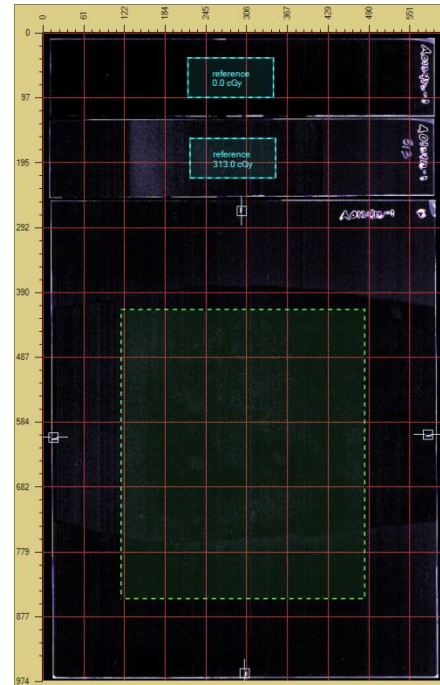
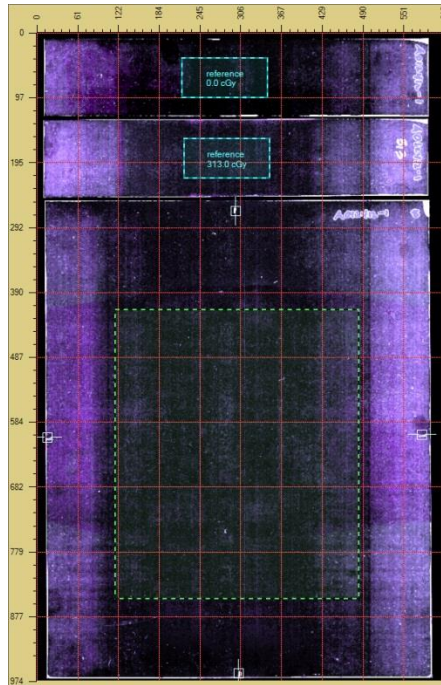
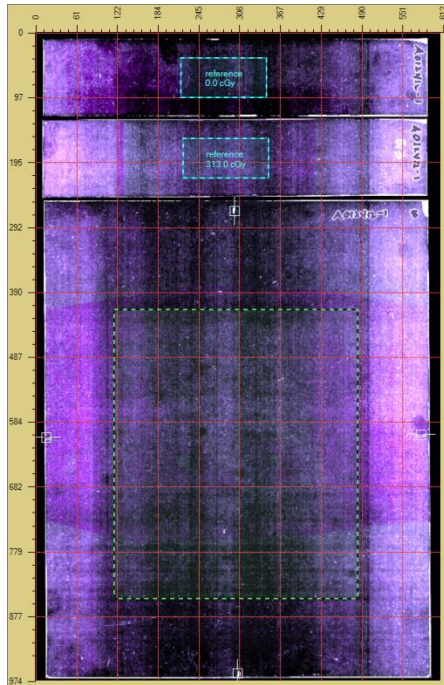


EBT3+ - Reference Recalibration

- Configuration same as EBT3
- Attached reference strip
 - Strip *properties as close as possible* to patient film
- Perforated Sheet
easy to detach reference strip
 - Saves film cutting
 - Standardized strip size
- EBT3+ available since 2012



Consistency Comparison



Single Channel

**10.2 cGy
4.2%**

**Single Channel
Recalibrated**

**3.6 cGy
1.5%**

Multi Channel

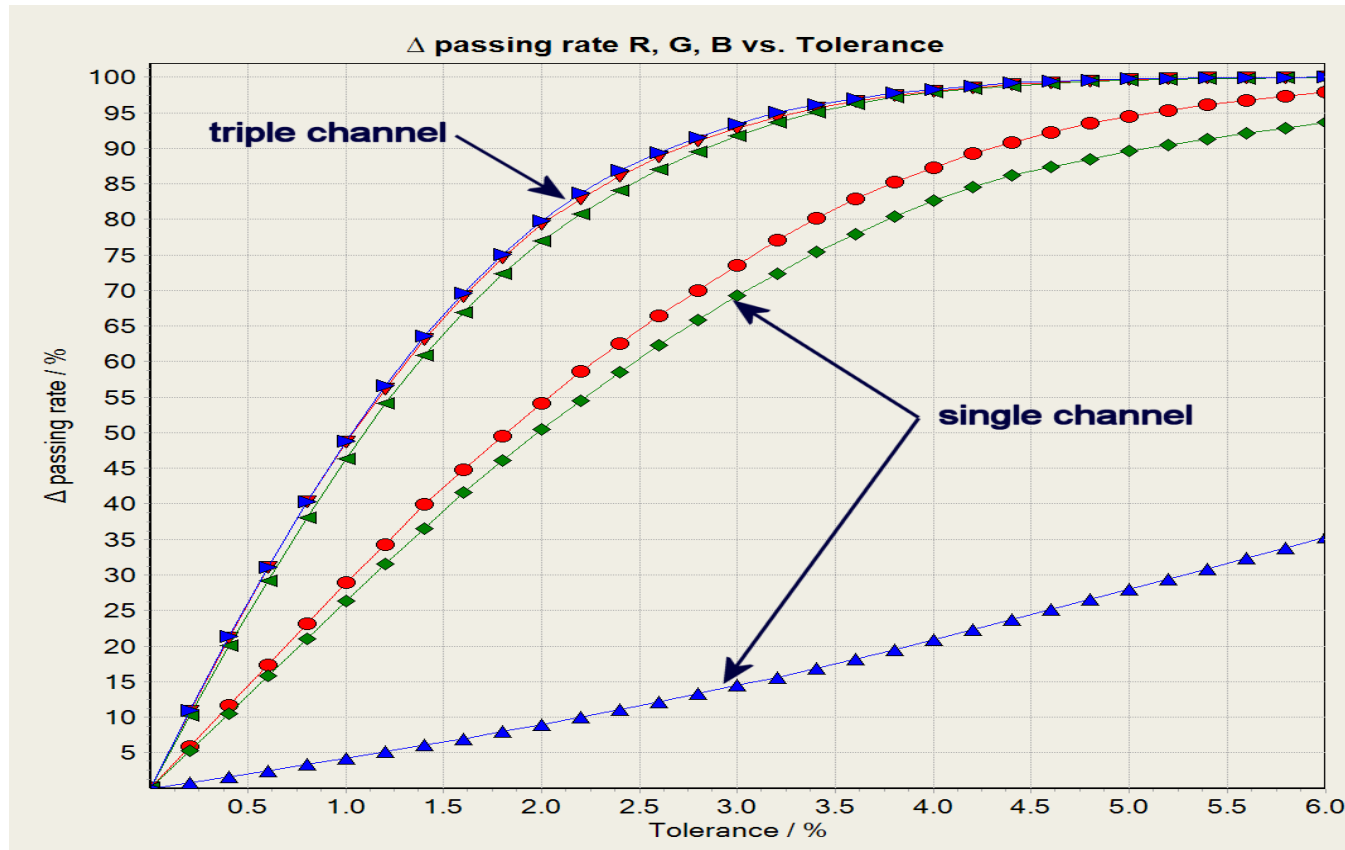
**1.3 cGy
0.53%**

**Multi Channel
Recalibrated**

**1.2 cGy
0.49%**

Consistency measured across frame $D_{\max} = 243 \text{ cGy}$, $D_{\text{ave}} = 139 \text{ cGy}$

Single vs Multi-Channel Comparison



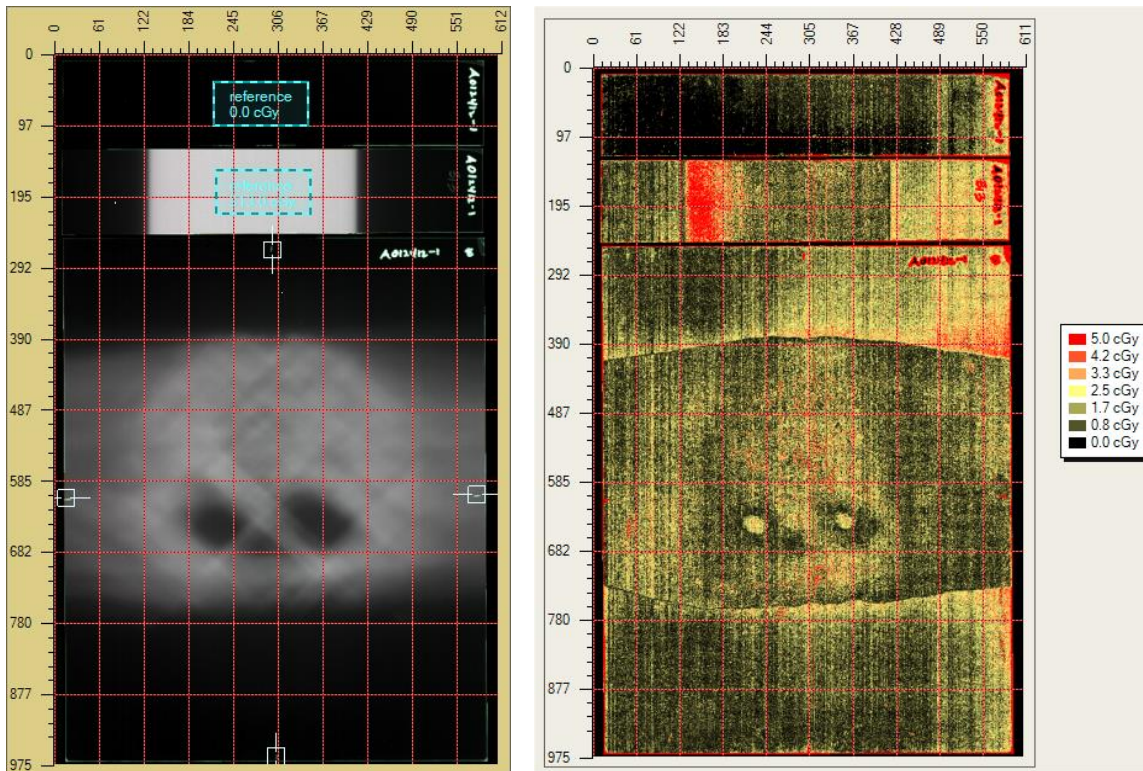
Differential pixel-wise direct comparison

- Multi channel: 90% passing rate at **2.7%** tolerance for All channels
- Single channel: 90% passing rate at **4.3%/5.1%/18.4%** RGB
- Multi channel method is consistent, single channel is Not

Multi-Channel Dosimetry

Dose Map Consistency

- Dose map error estimation known before comparison
- Detect 'abnormal' scans
 - 90° rotation, curling, Newton rings

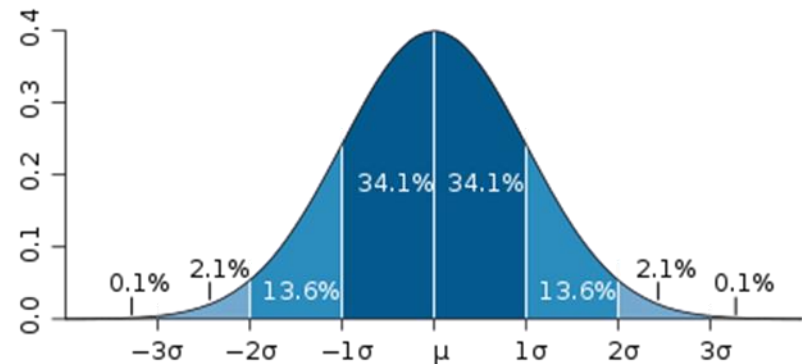


Example dose consistency map (iso-map) peak error $\sim 2\%$

Multi-Channel Film Dosimetry

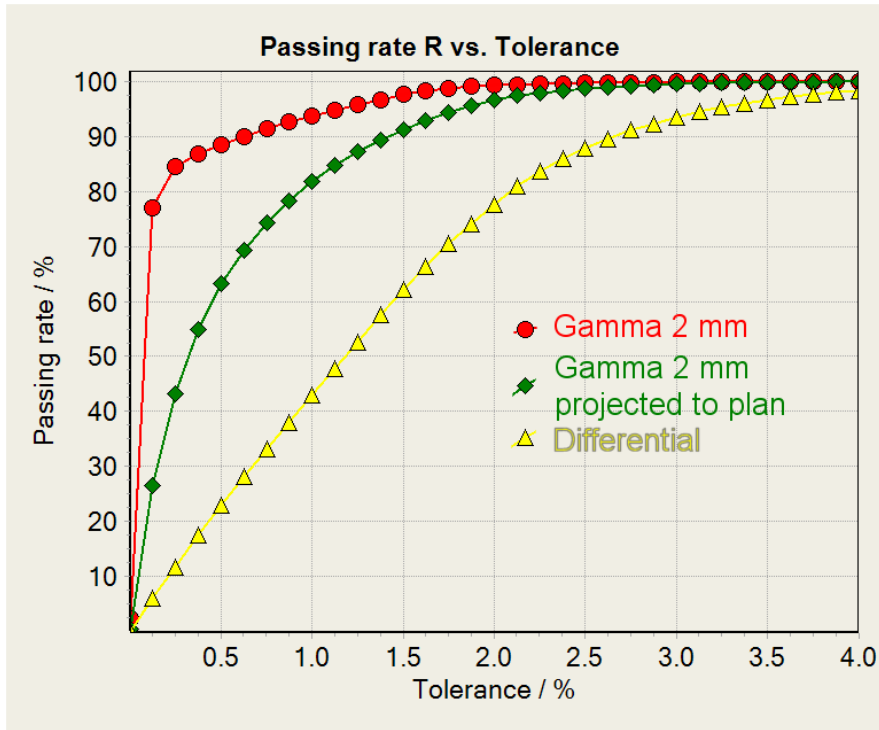
Dose to Plan Comparison

- ➔ Dose map error can dominate comparison
 - $\sim 0.5\%$ achievable (vs. 3% with single channel method)
- ➔ Comparison Criteria 3%/3mm, 2%/2mm
 - Triple channel: 1% \ll 3%/2%, *i.e.* majority $<$ tolerance
 - Single channel: 3% \sim 3% test, *i.e.* 50% $>$ tolerance
- ➔ Passing rates improves more than dose accuracy

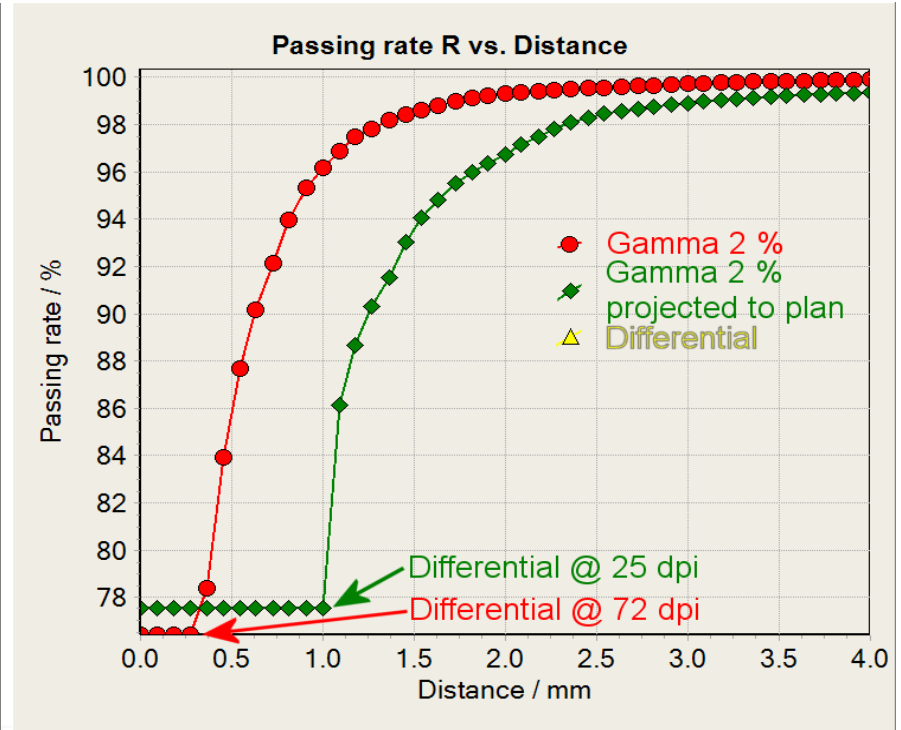


Gamma Map Comparison

Passing Rate Dependencies

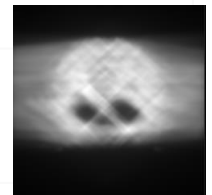


Passing Rate vs. Tolerance



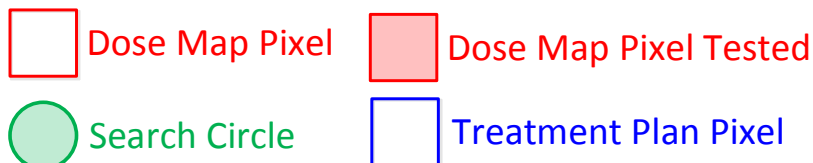
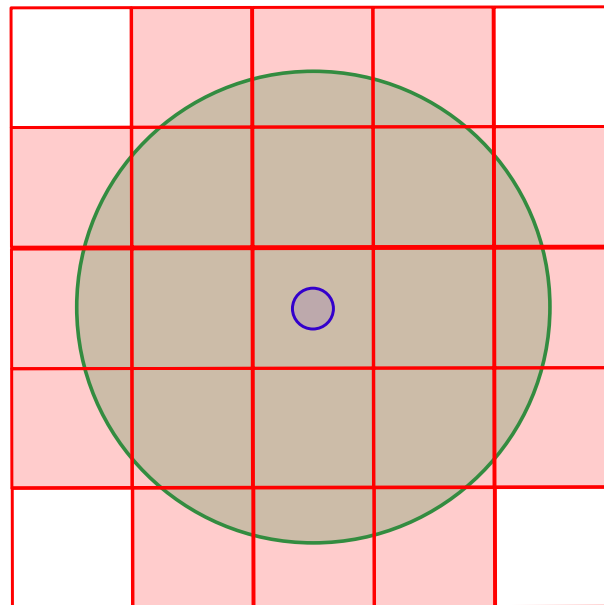
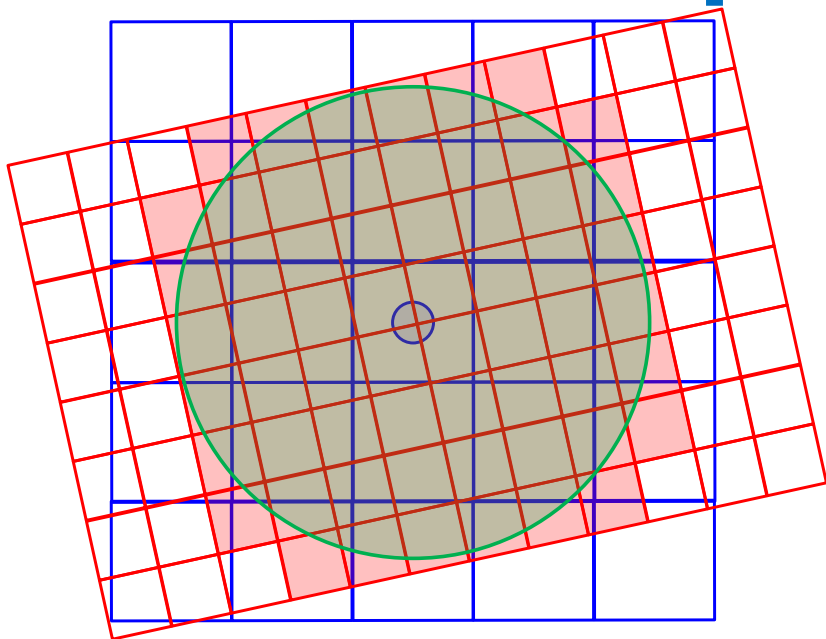
Passing Rate vs. Distance (DTA)

Gamma Map **2%/2mm** - FilmQA Pro RapidArc example
Distance dependence chart suggest **Resolution** dependence



Gamma Map Comparison

Dose Map Projection

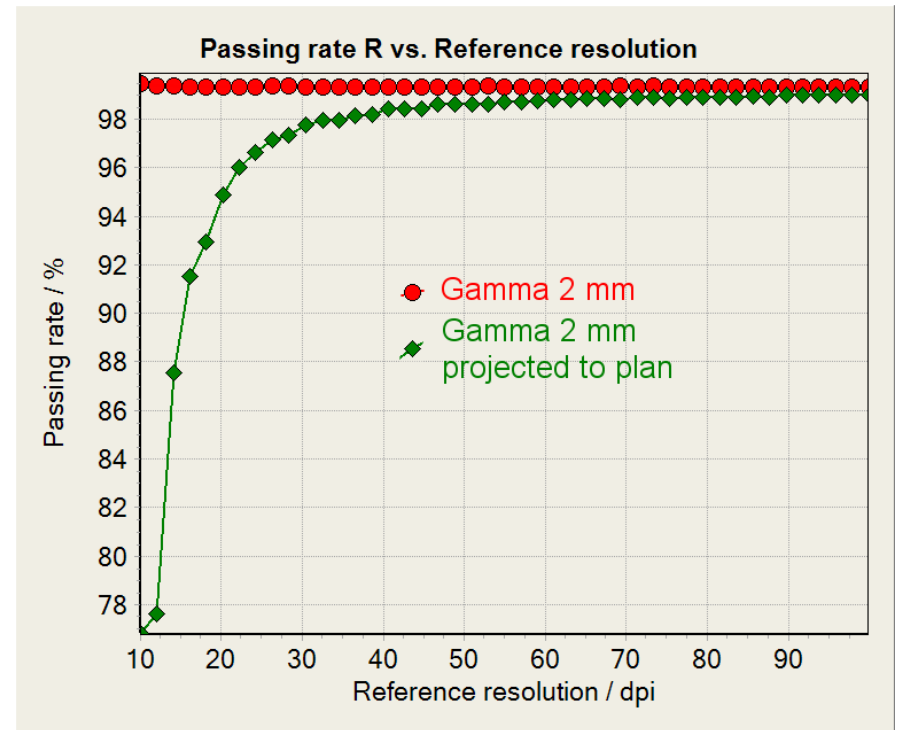
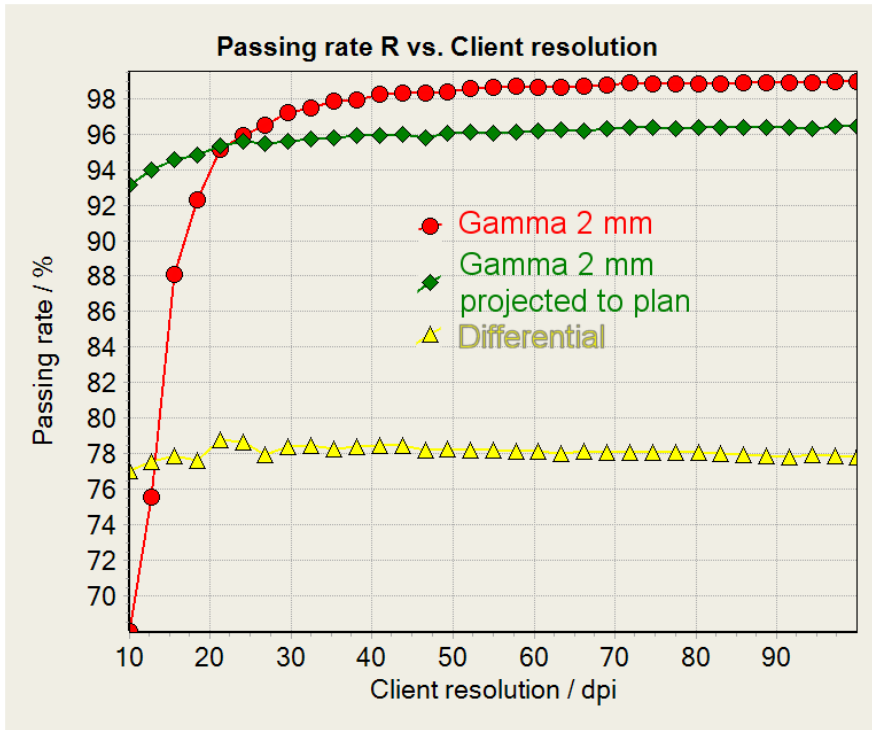


Gamma no projection

Gamma projected

Gamma Map Comparison

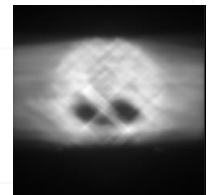
Passing Rate Dependencies



Passing Rate vs. Dose Map Resolution

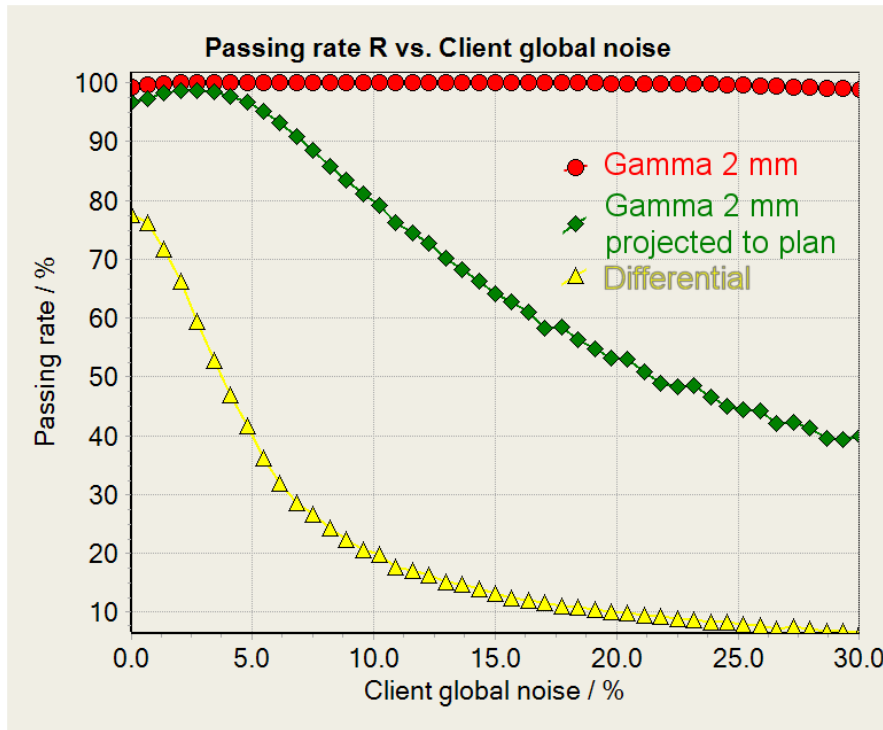
Passing Rate vs. Plan Resolution

Gamma Map **2%/2mm** - FilmQA Pro RapidArc example
 Passing rate R **99.3 %**

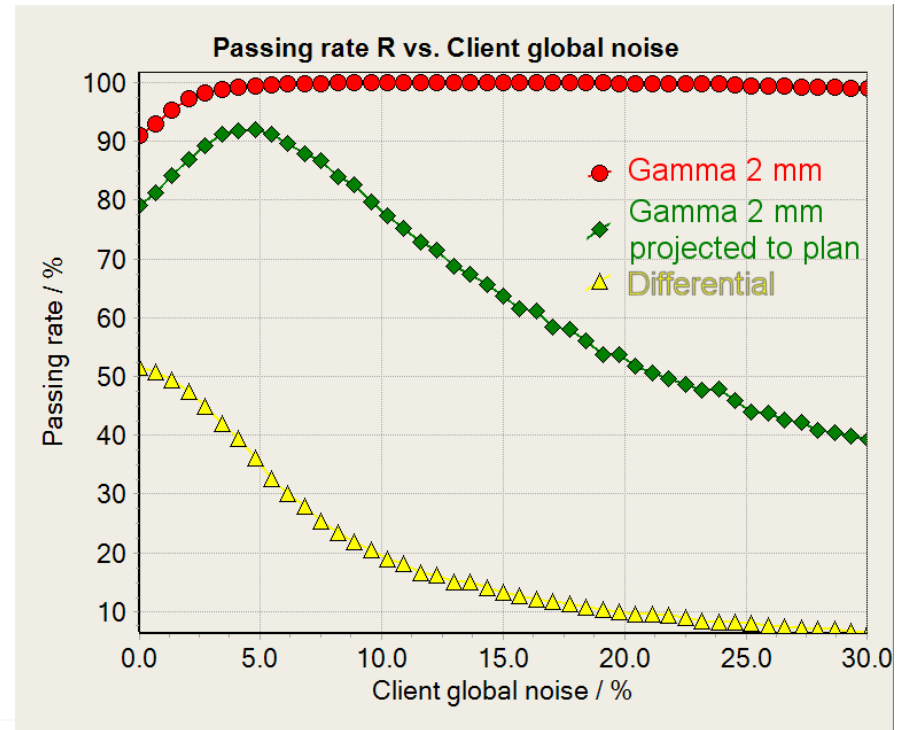


Gamma Map Comparison

Passing Rate Dependencies

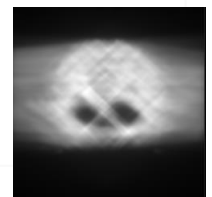


Passing Rate @ best location vs. Noise

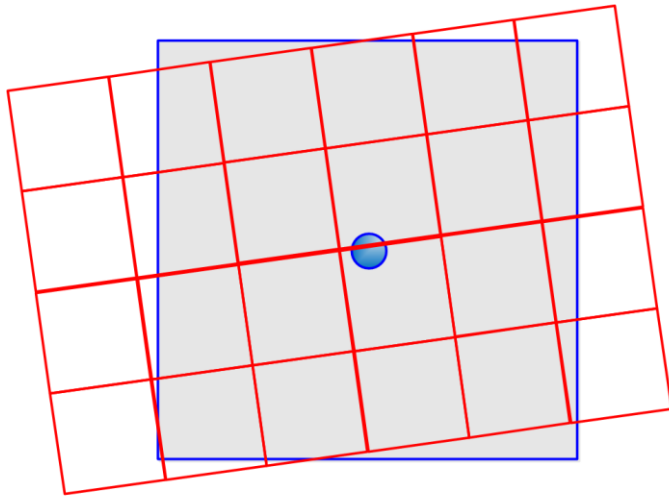


Passing Rate @ 2 mm shift vs. Noise

Gamma Map 2%/2mm - FilmQA Pro RapidArc example
 Equi-distributed noise added, x axis shows maximum amplitude



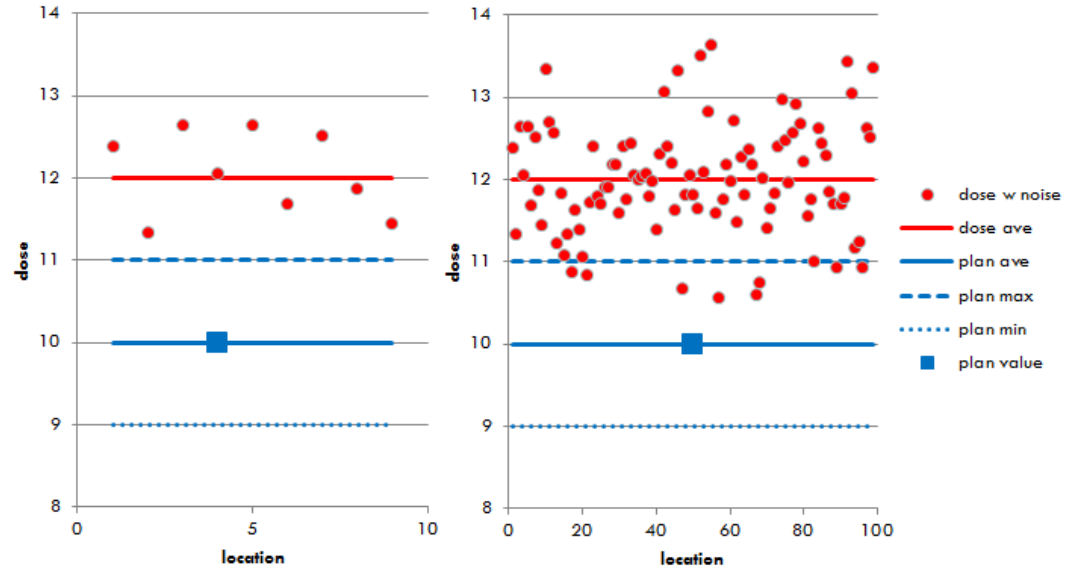
Gamma Map Comparison



 Dose Map Pixel

 Treatment Plan Pixel

plan pixel and overlaid pixels of registered dose map



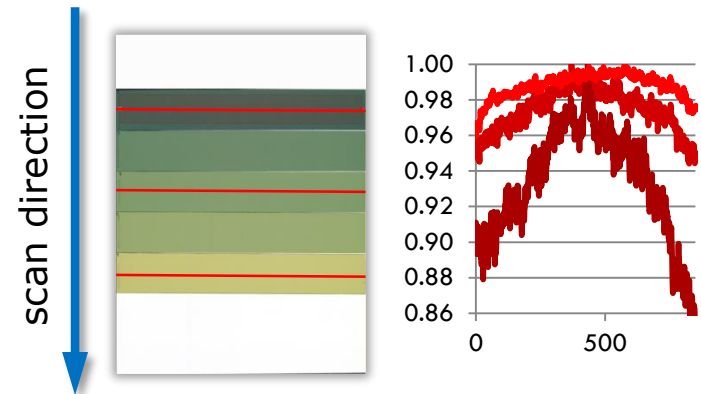
same standard deviation
low sample number **fails**,
high sample number **passes**

↪ Use dose average across plan pixel
e.g. Projection of dose map to plan coordinate system
Filtering cannot fix this problem!

Lateral Scanner Non-Linearity Normalized Blank Scan

Lateral effect increases with dose

- ➔ Compensates only weakest occurrence of lateral effect
- ➔ Adding disturbances
 - Non-uniformity of blank film
 - Noise of blank scan
- ➔ Worsens consistency for exposed areas
- ➔ Improved Gamma passing rates reported due to noise



Calibration patch consistency comparison

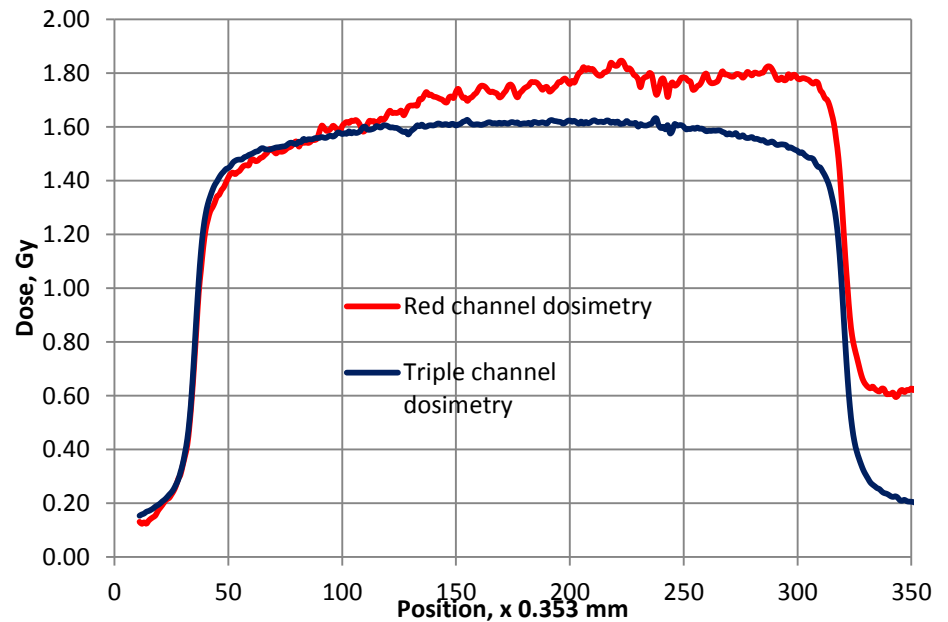
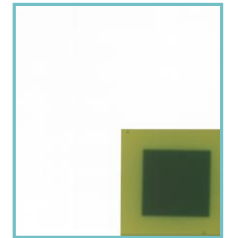
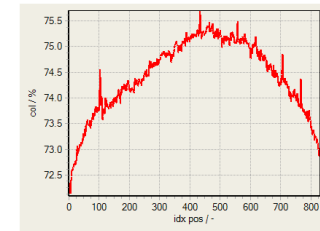
dose <cGy>	Consistency <cGy>		Consistency <%>	
	None	Blank scan	None	Blank scan
202.0	8.8	11.1	4.3	5.5
151.5	6.8	8.9	4.5	5.9
101.0	5.9	8.4	5.9	8.3
50.5	5.9	7.9	11.6	15.6
0.0	4.8	0.4	Infinity	Infinity

! DO NOT USE !

Triple Channel Dosimetry Lateral Scanner Non-Linearity

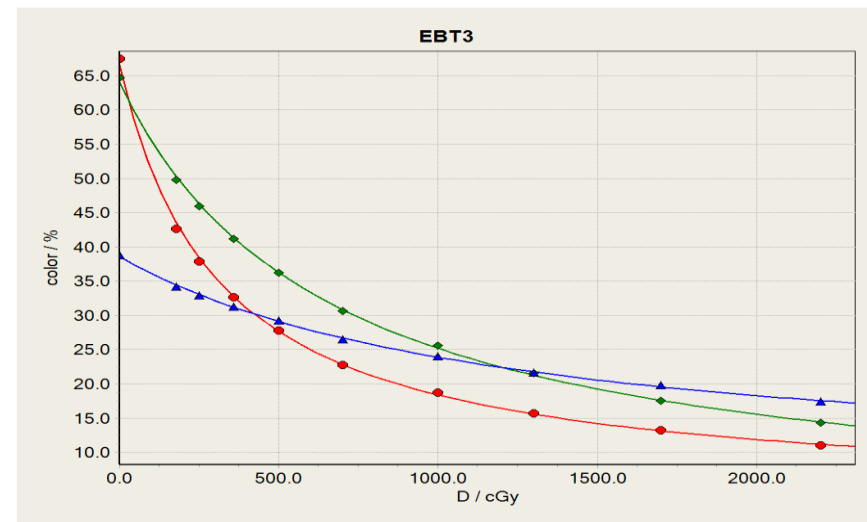
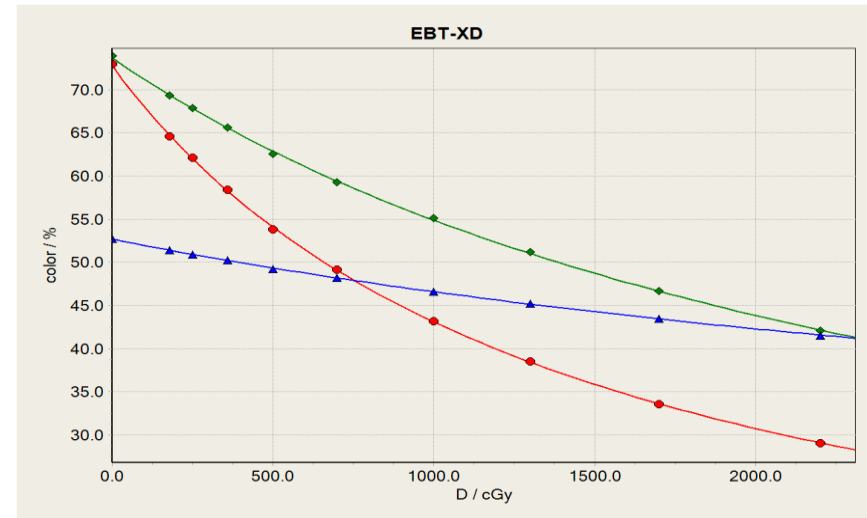
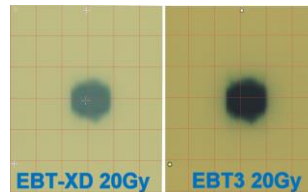
Scanner signal changes with lateral position (sensor direction)

- EBT film polarization causes lateral effect
- Non-dose-dependent part of lateral effect is compensated
- Mitigation only (partial compensation)



EBT-XD - Dose Range

- ➔ EBT-XD optical similar to EBT3 at 4x dose
 - Use at $D_{\max} > 20$ Gy
 - Wide fields use at $D_{\max} > 5$ Gy
 - High dose range better
Low dose range worse
- ➔ Format same as EBT3
- ➔ EBT-XD available since 2015/1



Multi-Channel - Dose Range Example

➔ SBRT 20Gy case

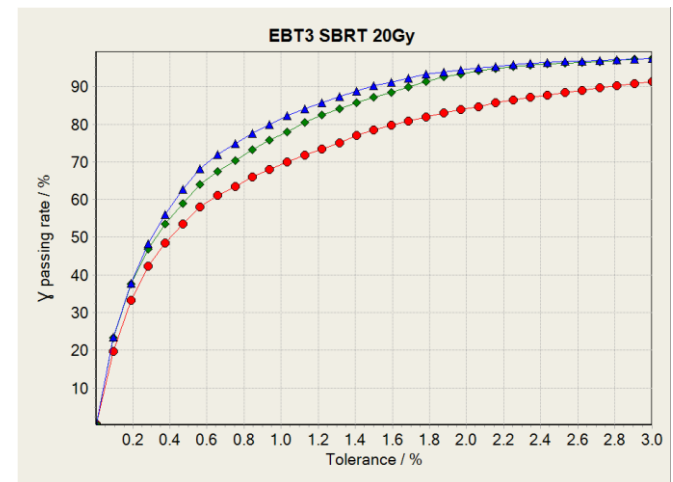
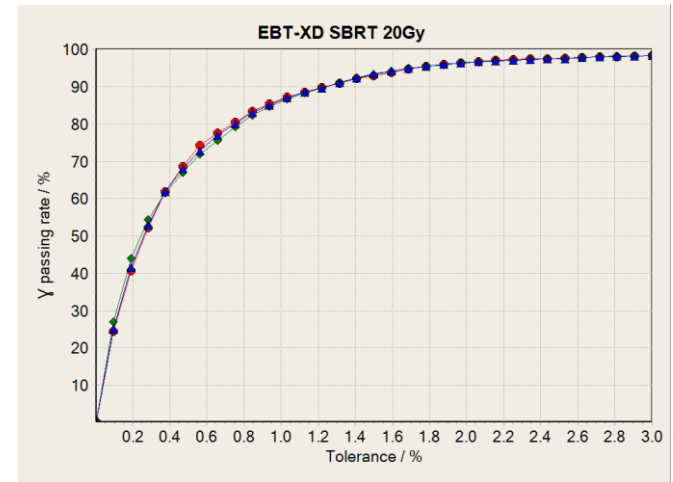
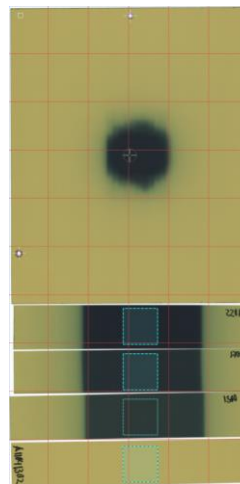
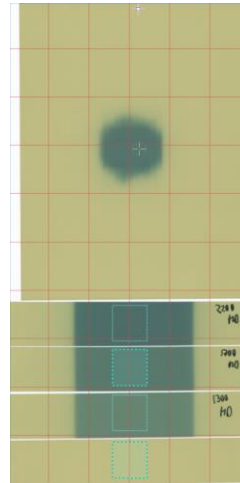
- Gamma 2 mm
- Tolerance to reach 90% passing rate

➔ EBT-XD

- Standard protocol
RGB 1.2/1.2/1.2%

➔ EBT3

- Standard protocol
RGB 2.8/1.7/1.5%
- With 2nd Reference
RGB 1.5/1.6/1.6%



Passing Rate vs Gamma Tolerance

Comparison Sensitivity

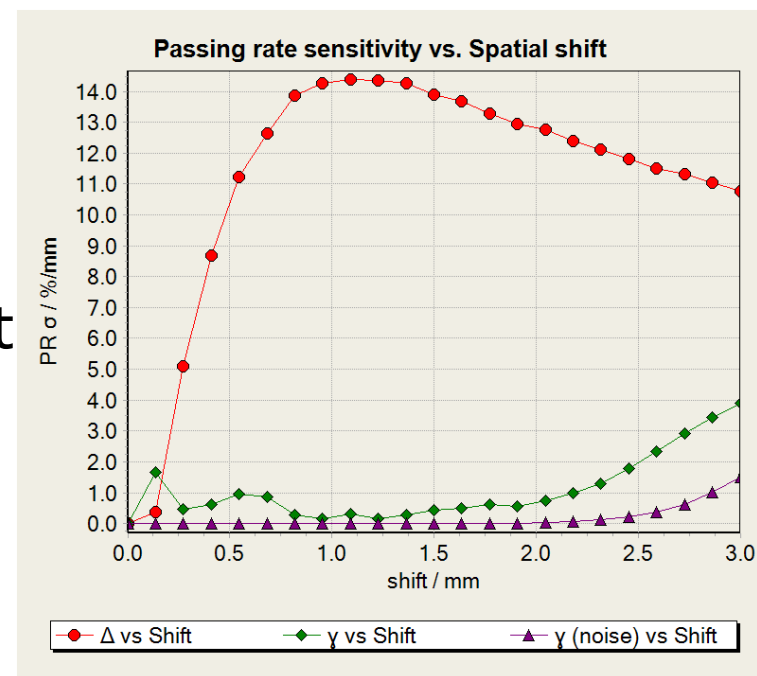
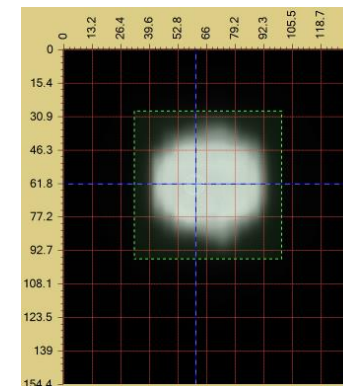
$$\text{Sensitivity} = \frac{\text{Change of Passing Rate}}{\text{Change of Disturbance}}$$

Ability of Comparison Map to QA specific Dose Disturbance

- Disturbance types
 - Spatial shift
 - Spatial rotation
 - Dose scaling
 - TPS calculated plan offset
- Random or Systematic

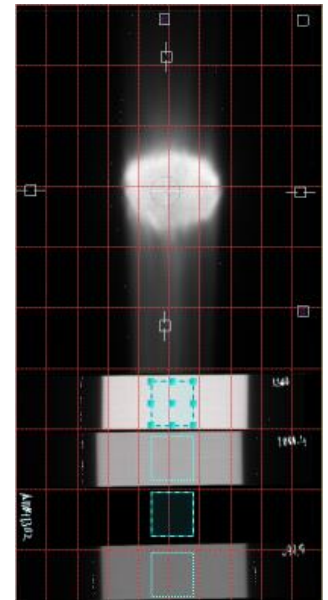
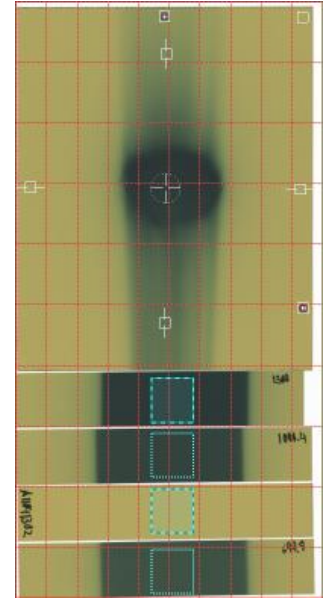
Example:

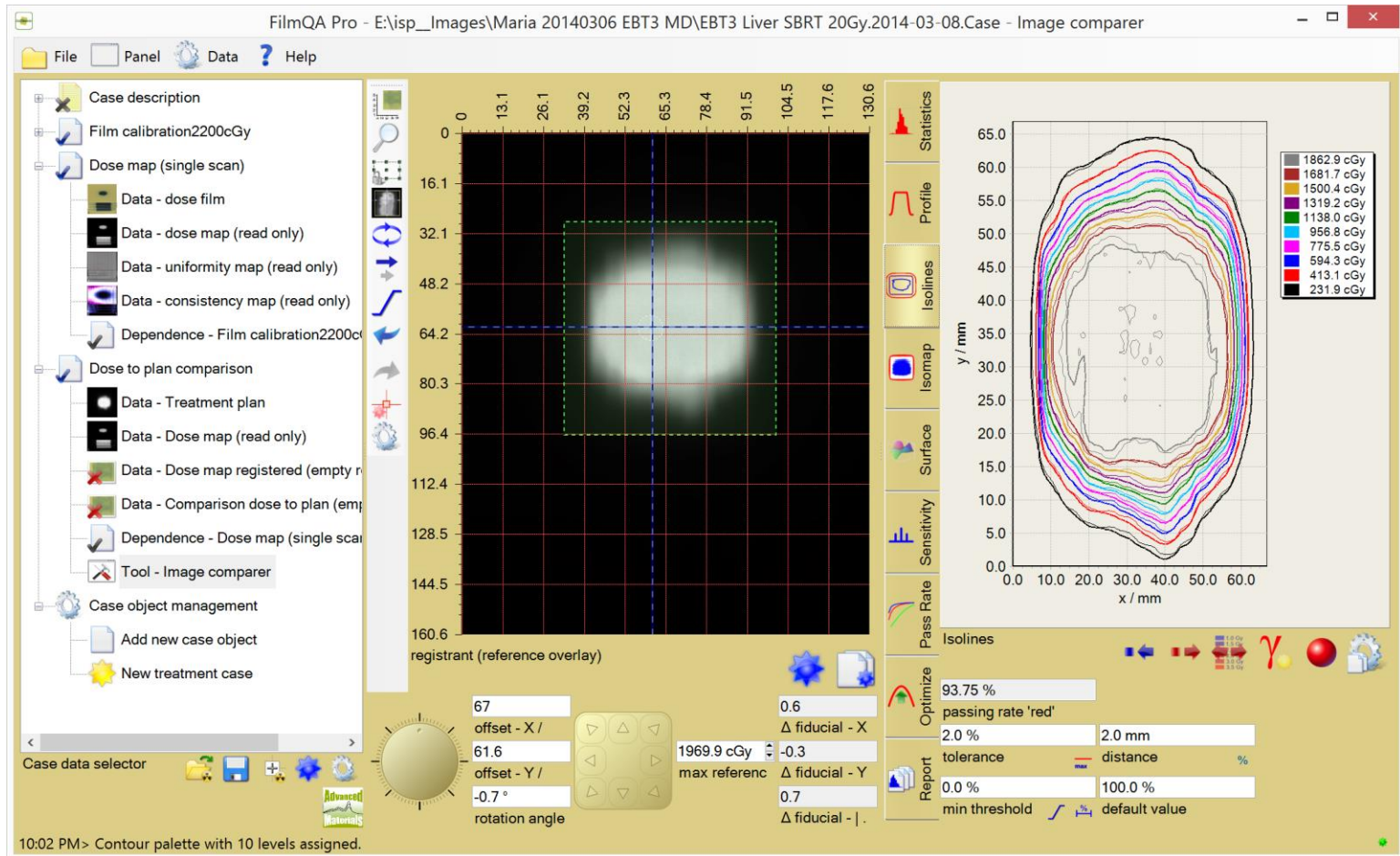
- SBRT $\sim 5 \times 5 \text{cm}^2$ field



GafChromic Protocol

- ➔ **Separate Dose and Dose-independent effects**
 - Compensates for film thickness variation
 - Mitigates scanner distortions
- ➔ **Enables entire film dose range**
 - Dynamic range ratio >1000
 - EBT2/EBT3 5 cGy - >20 Gy , EBT-XD 4x EBT3 range
- ➔ **Significant improvement of dose map accuracy**
 - ~0.5% routinely achievable
- ➔ **Consistency based estimation of dose error**
 - Active error improvement using reference exposures
- ➔ **Efficient workflow**
 - Package “Quick Phantom – EBT film – FilmQA Pro” enables best practice
 - Automatic registration using phantom fiducials
 - Evaluation 30 min after exposure possible





Micke, Lewis, Yu - Multi-channel Film Dosimetry with Non-Uniformity Correction, *Medical Physics*, 38 (2011) 5, pp. 2523.

Lewis, Micke, Yu, Chan - An Efficient Protocol for Radiochromic Film Dosimetry combining Calibration and Measurement in a Single Scan, *Medical Physics*, 39 (2012) 10, pp. 6339.